



US009445913B2

(12) **United States Patent**
Donner et al.

(10) **Patent No.:** **US 9,445,913 B2**
(45) **Date of Patent:** **Sep. 20, 2016**

(54) **ARCuate FIXATION MEMBER**

(71) Applicant: **DePuy Synthes Products, Inc.**,
Raynham, MA (US)

(72) Inventors: **Thomas Donner**, Thibodaux, LA (US);
Jared Schoenly, West Chester, PA
(US); **David Evans**, Cebu (PH);
Andreas Gfeller, Zofingen (CH)

(73) Assignee: **DePuy Synthes Products, Inc.**,
Raynham, MA (US)

(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 0 days.

2310/00359; A61F 2310/00017; A61F
2310/00023; A61F 2310/00131; A61F
2002/2835; A61F 2002/30387; A61F
2002/30509; A61F 2002/30514; A61F
2002/30517; A61F 2002/30578; A61F
2002/30604; A61F 2002/30616; A61F
2002/30777; A61F 2002/30784; A61F
2002/30787; A61F 2002/30841; A61F
2002/30843; A61F 2002/30845; A61F
2002/4475; A61F 2002/4627; A61F
2002/4628; A61F 2220/0025
USPC 623/17.11–17.16; 606/246–279,
606/300–310
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

(21) Appl. No.: **14/148,949**

(22) Filed: **Jan. 7, 2014**

4,790,303 A 12/1988 Steffee
5,263,953 A 11/1993 Bagby

(65) **Prior Publication Data**

US 2014/0163684 A1 Jun. 12, 2014

(Continued)

FOREIGN PATENT DOCUMENTS

Related U.S. Application Data

(63) Continuation of application No. 13/070,883, filed on
Mar. 24, 2011, now Pat. No. 8,641,766, which is a
continuation-in-part of application No. 12/761,101,
filed on Apr. 15, 2010.

(60) Provisional application No. 61/169,461, filed on Apr.
15, 2009.

CA 2279936 8/1998
CA 2279938 C 1/2006

(Continued)

OTHER PUBLICATIONS

U.S. Appl. No. 61/120,138, filed Dec. 5, 2008, Overes.

(Continued)

(51) **Int. Cl.**

A61F 2/44 (2006.01)

A61B 17/70 (2006.01)

(Continued)

Primary Examiner — Pedro Philogene

(74) *Attorney, Agent, or Firm* — Baker & Hostetler LLP

(52) **U.S. Cl.**

CPC **A61F 2/442** (2013.01); **A61B 17/70**
(2013.01); **A61B 17/7056** (2013.01);

(Continued)

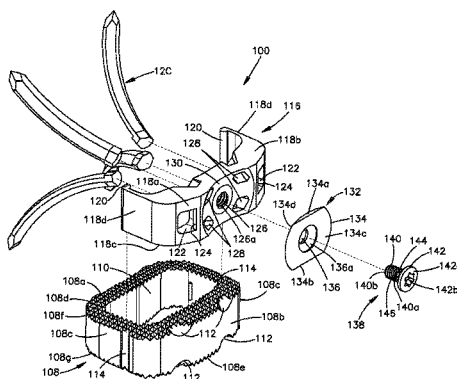
(57) **ABSTRACT**

Arcuate fixation members with varying configurations and/or features are provided, along with additional components for use therewith in provided intervertebral implants. The arcuate fixation members may be of different lengths, cross sectional geometries, and/or cross sectional areas. Applications of intervertebral implants utilizing arcuate fixation members are particularly suitable when a linear line-of-approach for delivering fixation members is undesirable.

(58) **Field of Classification Search**

CPC .. A61B 17/70; A61B 17/92; A61B 17/7056;
A61B 2017/8655; A61F 2/442; A61F 2/4455;
A61F 2/4611; A61F 2/28; A61F 2/30744;
A61F 2/30965; A61F 2/4465; A61F

19 Claims, 18 Drawing Sheets



(51)	Int. Cl.		6,953,462 B2	10/2005	Lieberman
	<i>A61B 17/92</i>	(2006.01)	6,969,390 B2	11/2005	Michelson
	<i>A61F 2/46</i>	(2006.01)	7,037,340 B2	5/2006	Gau
	<i>A61B 17/86</i>	(2006.01)	7,041,135 B2	5/2006	Michelson
	<i>A61F 2/28</i>	(2006.01)	7,051,610 B2	5/2006	Stoianovici et al.
	<i>A61F 2/30</i>	(2006.01)	7,056,344 B2	6/2006	Huppert et al.
(52)	U.S. Cl.		7,074,221 B2	7/2006	Michelson
	CPC <i>A61B 17/92</i> (2013.01); <i>A61F 2/4455</i>		7,077,844 B2	7/2006	Michelson
	(2013.01); <i>A61F 2/4611</i> (2013.01); <i>A61B</i>		7,137,984 B2	11/2006	Michelson
	<i>2017/8655</i> (2013.01); <i>A61F 2/28</i> (2013.01);		7,172,627 B2	2/2007	Fiere et al.
	<i>A61F 2/30744</i> (2013.01); <i>A61F 2/30965</i>		7,195,643 B2	3/2007	Jackson
	(2013.01); <i>A61F 2/4465</i> (2013.01); <i>A61F</i>		7,255,698 B2	8/2007	Michelson
	<i>2002/2835</i> (2013.01); <i>A61F 2002/30387</i>		7,291,170 B2	11/2007	Huppert
	(2013.01); <i>A61F 2002/30509</i> (2013.01); <i>A61F</i>		7,326,250 B2	2/2008	Beaurain et al.
	<i>2002/30514</i> (2013.01); <i>A61F 2002/30517</i>		7,455,684 B2	11/2008	Gradel et al.
	(2013.01); <i>A61F 2002/30578</i> (2013.01); <i>A61F</i>		7,494,508 B2	2/2009	Zeegers
	<i>2002/30604</i> (2013.01); <i>A61F 2002/30616</i>		7,507,248 B2	3/2009	Beaurain et al.
	(2013.01); <i>A61F 2002/30777</i> (2013.01); <i>A61F</i>		7,594,931 B2	9/2009	Louis et al.
	<i>2002/30784</i> (2013.01); <i>A61F 2002/30787</i>		7,625,381 B2	12/2009	Michelson
	(2013.01); <i>A61F 2002/30841</i> (2013.01); <i>A61F</i>		7,632,282 B2	12/2009	Dinville
	<i>2002/30843</i> (2013.01); <i>A61F 2002/30845</i>		7,651,497 B2	1/2010	Michelson
	(2013.01); <i>A61F 2002/4475</i> (2013.01); <i>A61F</i>		7,662,182 B2	2/2010	Zubok et al.
	<i>2002/4627</i> (2013.01); <i>A61F 2002/4628</i>		7,662,185 B2	2/2010	Alfaro et al.
	(2013.01); <i>A61F 2220/0025</i> (2013.01); <i>A61F</i>		7,682,396 B2	3/2010	Beaurain et al.
	<i>2310/00017</i> (2013.01); <i>A61F 2310/00023</i>		7,695,516 B2	4/2010	Zeegers
	(2013.01); <i>A61F 2310/00131</i> (2013.01); <i>A61F</i>		7,695,518 B2	4/2010	Gau
	<i>2310/00359</i> (2013.01)		7,704,255 B2	4/2010	Michelson
			7,842,088 B2	11/2010	Rashbaum et al.
			7,846,188 B2	12/2010	Moskowitz et al.
			8,002,835 B2	8/2011	Zeegers
			8,075,618 B2	12/2011	Trieu et al.
			8,147,556 B2	4/2012	Louis et al.
			8,162,988 B2	4/2012	Delecrin et al.
			8,221,422 B2	7/2012	Mangione
			8,221,457 B2	7/2012	Delecrin et al.
			8,241,359 B2	8/2012	Davis et al.
			8,257,439 B2	9/2012	Zeegers
			8,257,443 B2	9/2012	Kamran et al.
			8,262,700 B2	9/2012	Cho et al.
			8,267,999 B2	9/2012	Beaurain et al.
			8,303,663 B2	11/2012	Jimenez et al.
			8,313,528 B1	11/2012	Wensel
			8,323,345 B2	12/2012	Sledge
			8,328,872 B2	12/2012	Duffield et al.
			8,333,804 B1 *	12/2012	Wensel <i>A61B 17/864</i> 623/17.11
			8,343,197 B2	1/2013	Gonzalez-Hernandez
			8,343,219 B2	1/2013	Allain et al.
			8,353,219 B2	1/2013	Brackett et al.
			8,409,288 B2	4/2013	Davis et al.
			8,430,915 B2	4/2013	Beaurain et al.
			8,439,931 B2	5/2013	Dinville
			8,465,546 B2	6/2013	Jodaitis et al.
			8,641,766 B2	2/2014	Donner et al.
			2002/0059938 A1	5/2002	Fogarty et al.
			2003/0195627 A1	10/2003	Ralph et al.
			2004/0054411 A1	3/2004	Kelly et al.
			2004/0068258 A1	4/2004	Schlapfer et al.
			2004/0082953 A1	4/2004	Petit
			2004/0093087 A1	5/2004	Ferree et al.
			2004/0210219 A1	10/2004	Bray
			2005/0101960 A1	5/2005	Fiere et al.
			2005/0107788 A1	5/2005	Beaurain et al.
			2005/0197706 A1	9/2005	Hovorka et al.
			2005/0251258 A1	11/2005	Jackson
			2006/0030851 A1	2/2006	Bray et al.
			2006/0085071 A1 *	4/2006	Lechmann <i>A61F 2/4455</i> 623/17.11
			2006/0271053 A1	11/2006	Schlapfer et al.
			2006/0282074 A1	12/2006	Renaud et al.
			2007/0016295 A1	1/2007	Boyd
			2007/0049943 A1	3/2007	Moskowitz et al.
			2007/0106388 A1	5/2007	Michelson
			2007/0162130 A1	7/2007	Rashbaum et al.
			2007/0208345 A1	9/2007	Marnay et al.
			2007/0270960 A1	11/2007	Bonin et al.
			2007/0270961 A1	11/2007	Ferguson
			2008/0021562 A1	1/2008	Huppert
			2008/0033432 A1	2/2008	McGraw et al.
(56)	References Cited				
	U.S. PATENT DOCUMENTS				
	5,300,074 A	4/1994 Frigg			
	5,401,269 A	3/1995 Buttner-Janz et al.			
	5,458,638 A	10/1995 Kuslich et al.			
	5,609,635 A *	3/1997 Michelson <i>A61F 2/30744</i> 606/247			
	5,888,223 A	3/1999 Bray, Jr.			
	5,899,905 A	5/1999 Errico et al.			
	6,036,701 A	3/2000 Rosenman			
	6,120,503 A	9/2000 Michelson			
	6,136,001 A	10/2000 Michelson			
	6,139,550 A	10/2000 Michelson			
	6,193,721 B1	2/2001 Michelson			
	6,231,610 B1	5/2001 Geisler			
	6,235,059 B1	5/2001 Benezech et al.			
	6,258,089 B1	7/2001 Campbell et al.			
	6,364,880 B1	4/2002 Michelson			
	6,383,186 B1	5/2002 Michelson			
	6,398,783 B1	6/2002 Michelson			
	6,413,259 B1	7/2002 Lyons et al.			
	6,416,528 B1	7/2002 Michelson			
	6,423,063 B1	7/2002 Bonutti			
	6,428,542 B1	8/2002 Michelson			
	6,432,106 B1	8/2002 Fraser			
	6,447,546 B1	9/2002 Bramlet et al.			
	6,454,771 B1	9/2002 Michelson			
	6,468,309 B1	10/2002 Lieberman			
	6,527,774 B2	3/2003 Lieberman			
	6,527,776 B1	3/2003 Michelson			
	6,551,319 B2	4/2003 Lieberman			
	6,558,423 B1	5/2003 Michelson			
	6,592,586 B1	7/2003 Michelson			
	6,616,666 B1	9/2003 Michelson			
	6,620,163 B1	9/2003 Michelson			
	6,626,907 B2	9/2003 Campbell et al.			
	6,695,846 B2	2/2004 Richelsoph et al.			
	6,712,818 B1	3/2004 Michelson			
	6,770,096 B2	8/2004 Bolger et al.			
	6,916,320 B2	7/2005 Michelson			
	6,926,718 B1	8/2005 Michelson			
	6,936,050 B2	8/2005 Michelson			
	6,936,051 B2	8/2005 Michelson			

(56)

References Cited

FOREIGN PATENT DOCUMENTS

U.S. PATENT DOCUMENTS

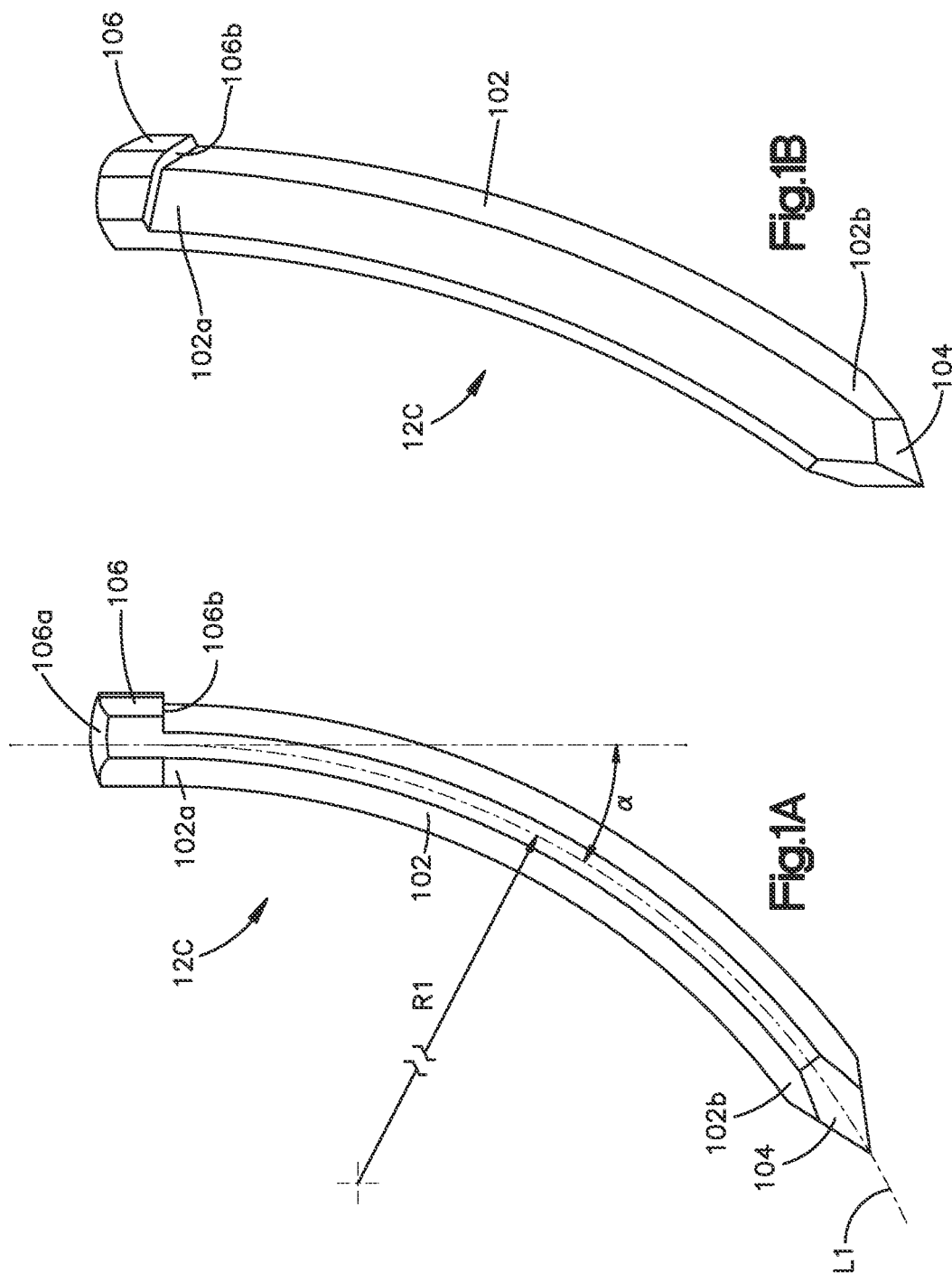
2008/0132949	A1	6/2008	Aferzon et al.	
2008/0234686	A1	9/2008	Beaurain et al.	
2008/0249625	A1	10/2008	Waugh et al.	
2008/0269768	A1	10/2008	Schwager et al.	
2008/0281425	A1	11/2008	Thalgott et al.	
2008/0306596	A1	12/2008	Jones et al.	
2008/0312742	A1	12/2008	Abernathie	
2008/0312743	A1	12/2008	Vila et al.	
2009/0054988	A1*	2/2009	Hess	A61B 17/025 623/17.16
2009/0105830	A1	4/2009	Jones et al.	
2009/0105831	A1	4/2009	Jones et al.	
2009/0105832	A1*	4/2009	Allain et al.	623/17.16
2009/0118771	A1	5/2009	Gonzalez-Hernandez	
2009/0149959	A1	6/2009	Conner et al.	
2009/0164020	A1*	6/2009	Janowski	A61F 2/4465 623/17.16
2009/0210062	A1*	8/2009	Thalgott et al.	623/17.16
2009/0210064	A1	8/2009	Lechmann et al.	
2009/0265007	A1	10/2009	Colleran	
2010/0010547	A1	1/2010	Beaurain et al.	
2010/0016974	A1	1/2010	Janowski et al.	
2010/0050276	A1	2/2010	DePaepe	
2010/0057206	A1	3/2010	Duffield et al.	
2010/0145460	A1	6/2010	McDonough et al.	
2010/0161057	A1	6/2010	Berry et al.	
2010/0185289	A1	7/2010	Kirwan et al.	
2010/0234958	A1*	9/2010	Linares	623/17.16
2010/0280618	A1	11/2010	Jodaitis et al.	
2010/0298941	A1	11/2010	Hes et al.	
2010/0312345	A1	12/2010	Duffield et al.	
2010/0312346	A1	12/2010	Kueenzi et al.	
2011/0077739	A1	3/2011	Rashbaum et al.	
2011/0112587	A1	5/2011	Patel et al.	
2011/0178599	A1	7/2011	Brett	
2011/0208311	A1	8/2011	Janowski	
2011/0230971	A1	9/2011	Donner	
2012/0022654	A1	1/2012	Farris et al.	
2012/0053693	A1	3/2012	Zeegers	
2012/0116466	A1	5/2012	Dinville et al.	
2012/0191196	A1	7/2012	Louis et al.	
2012/0197404	A1	8/2012	Brun et al.	
2012/0265248	A1	10/2012	Delecrin et al.	
2012/0310356	A1	12/2012	Davis et al.	
2012/0330424	A1	12/2012	Zeegers	
2013/0013006	A1	1/2013	Rashbaum et al.	
2013/0041408	A1	2/2013	Dinville et al.	
2013/0150968	A1	6/2013	Dinville et al.	
2013/0166029	A1	6/2013	Dinville et al.	
2013/0226300	A1	8/2013	Chataigner et al.	
2013/0253648	A1	9/2013	Beaurain et al.	
2013/0253651	A1	9/2013	Dinville	

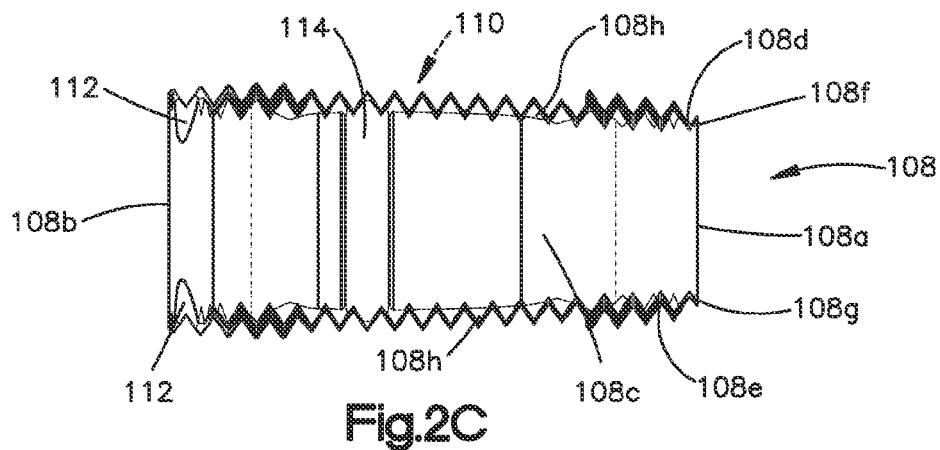
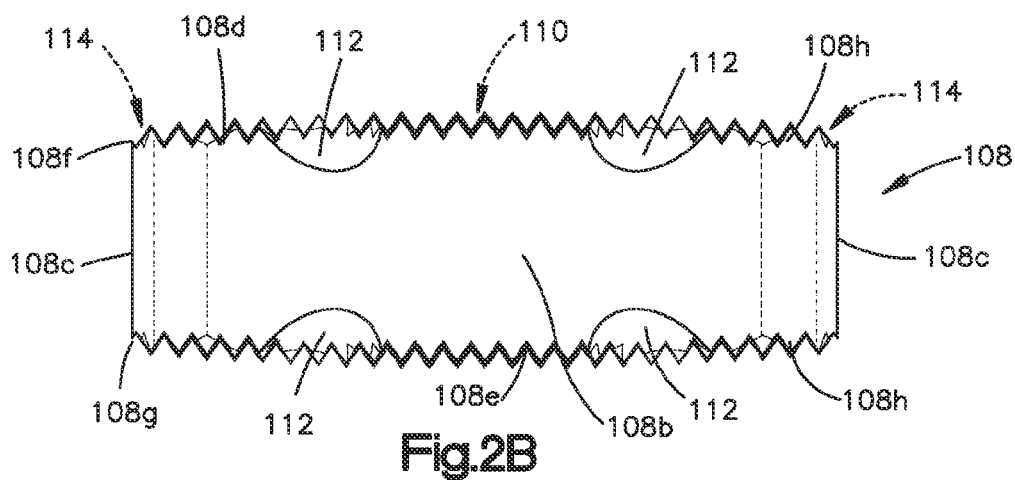
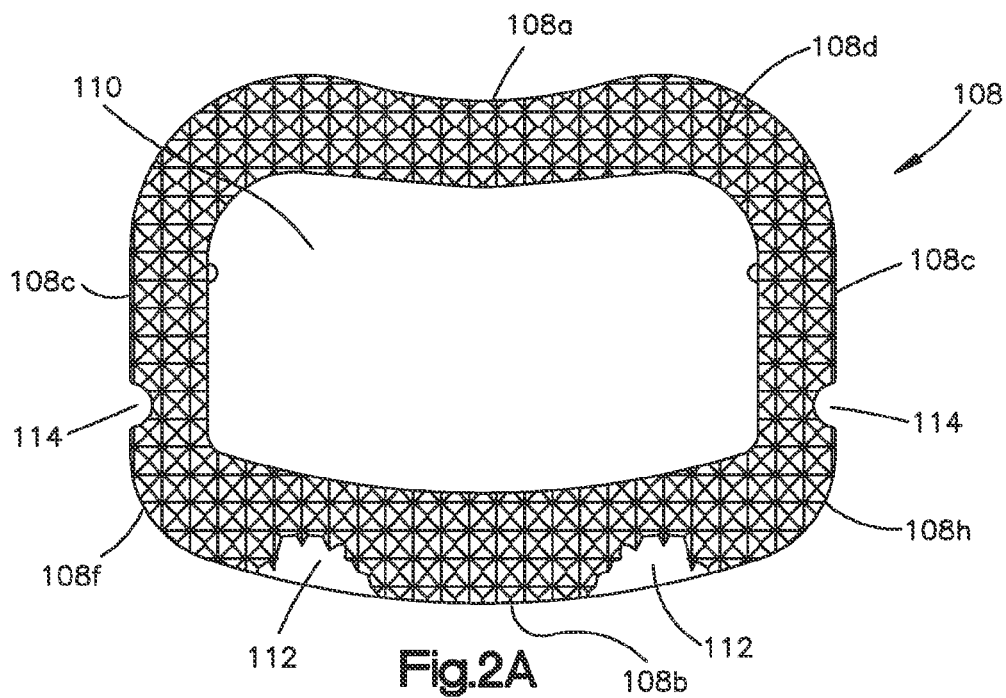
CA	2445299	C	1/2006
CA	2445303	C	1/2006
CA	2445319	C	1/2006
CA	2444232	C	4/2006
CA	2444222	C	5/2006
CA	2444226	C	6/2006
CA	2523814	C	2/2007
CA	2533689	C	5/2007
CA	2533699	C	5/2007
CA	2533695	C	6/2007
CA	2533713	C	6/2007
CN	1620271		5/2005
CN	201244104		5/2009
EP	1402836	B1	3/2004
EP	1006913	B1	11/2005
EP	0891169	B1	12/2005
EP	1006913	B8	1/2006
EP	1690508	A2	8/2006
EP	1393687	B1	1/2007
EP	1393688	B1	4/2007
EP	1393689	B1	8/2007
EP	1847229	A2	10/2007
EP	1402833	B1	5/2008
EP	1006913	B2	3/2009
EP	1402834	B1	1/2010
EP	1402832	B1	4/2011
EP	1402835	B1	9/2011
EP	2162098	B1	8/2015
FR	2727003		5/1996
FR	2848408		6/2004
FR	2916956		12/2008
JP	A-H07-008514		1/1995
JP	2001-252283		9/2001
JP	A-2003-516174		5/2003
JP	A-2004-500156		1/2004
JP	2006-510462		3/2006
JP	A-2006-513752		4/2006
WO	WO 2002/13732		2/2002
WO	WO 2004/093767		11/2004
WO	WO 2005/092219		10/2005
WO	WO 2007/098288		8/2007
WO	WO 2008/102174		8/2008
WO	WO 2009/004625		1/2009
WO	WO 2009/131955		10/2009
WO	WO 2010028045		3/2010
WO	WO 2010/121028		10/2010
WO	WO 2011/129973		10/2011

OTHER PUBLICATIONS

U.S. Appl. No. 61/169,461, filed Apr. 15, 2009, Laurence.
 International Patent Application No. PCT/US2010/031244: Inter-
 national Search Report dated Nov. 3, 2010, 10 pages.
 International Patent Application No. PCT/US2011/029738: Inter-
 national Search Report dated Jun. 29, 2011, 12 pages.

* cited by examiner





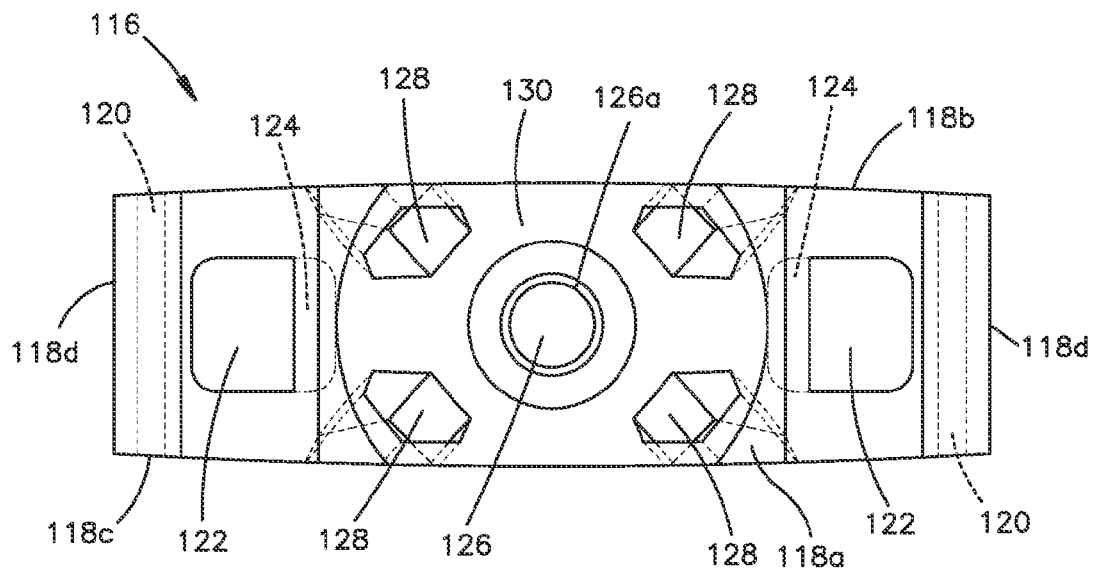


Fig.3A

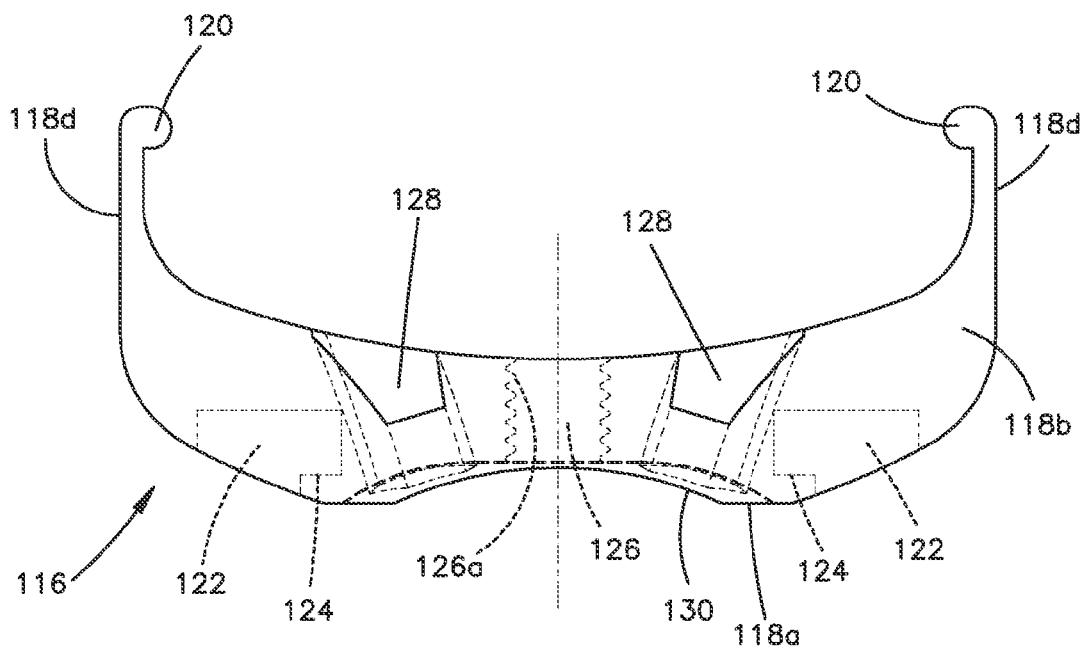


Fig.3B

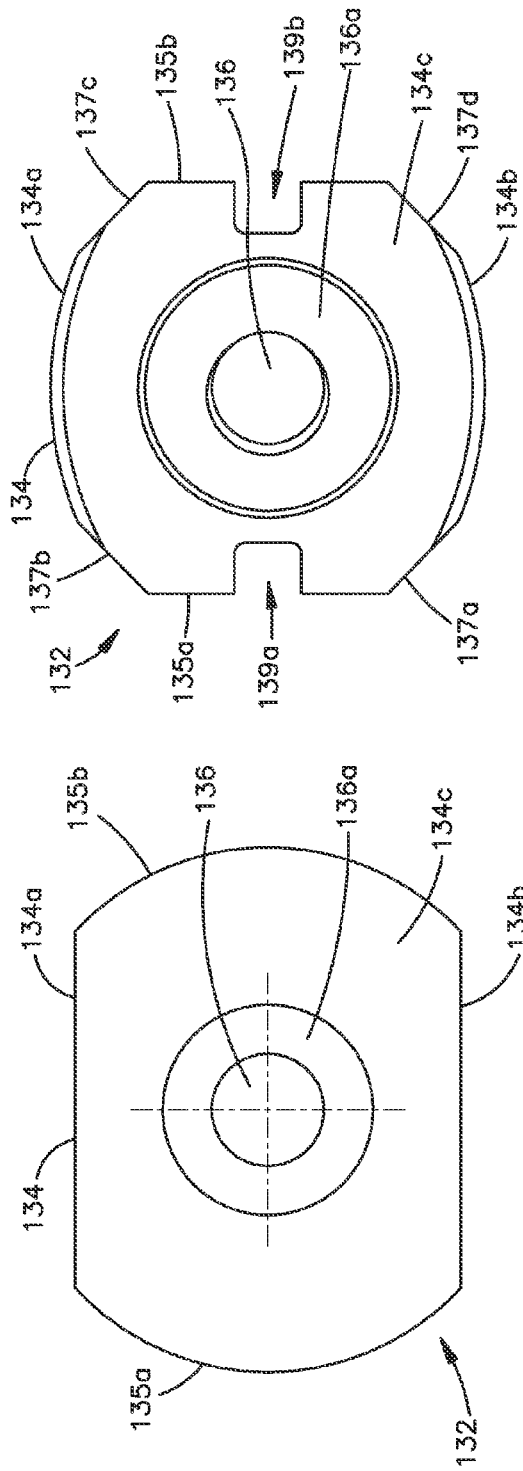


Fig. 4C

Fig. 4A

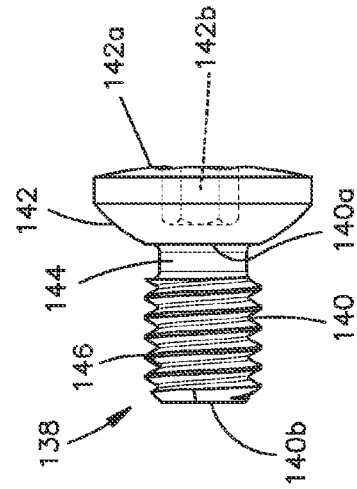


Fig. 5

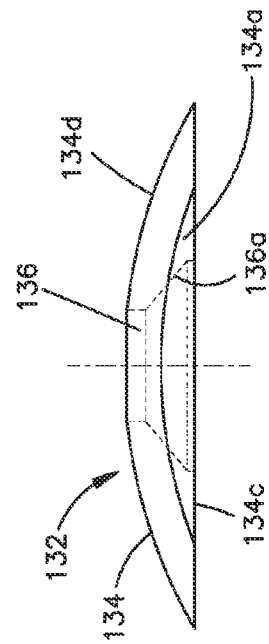
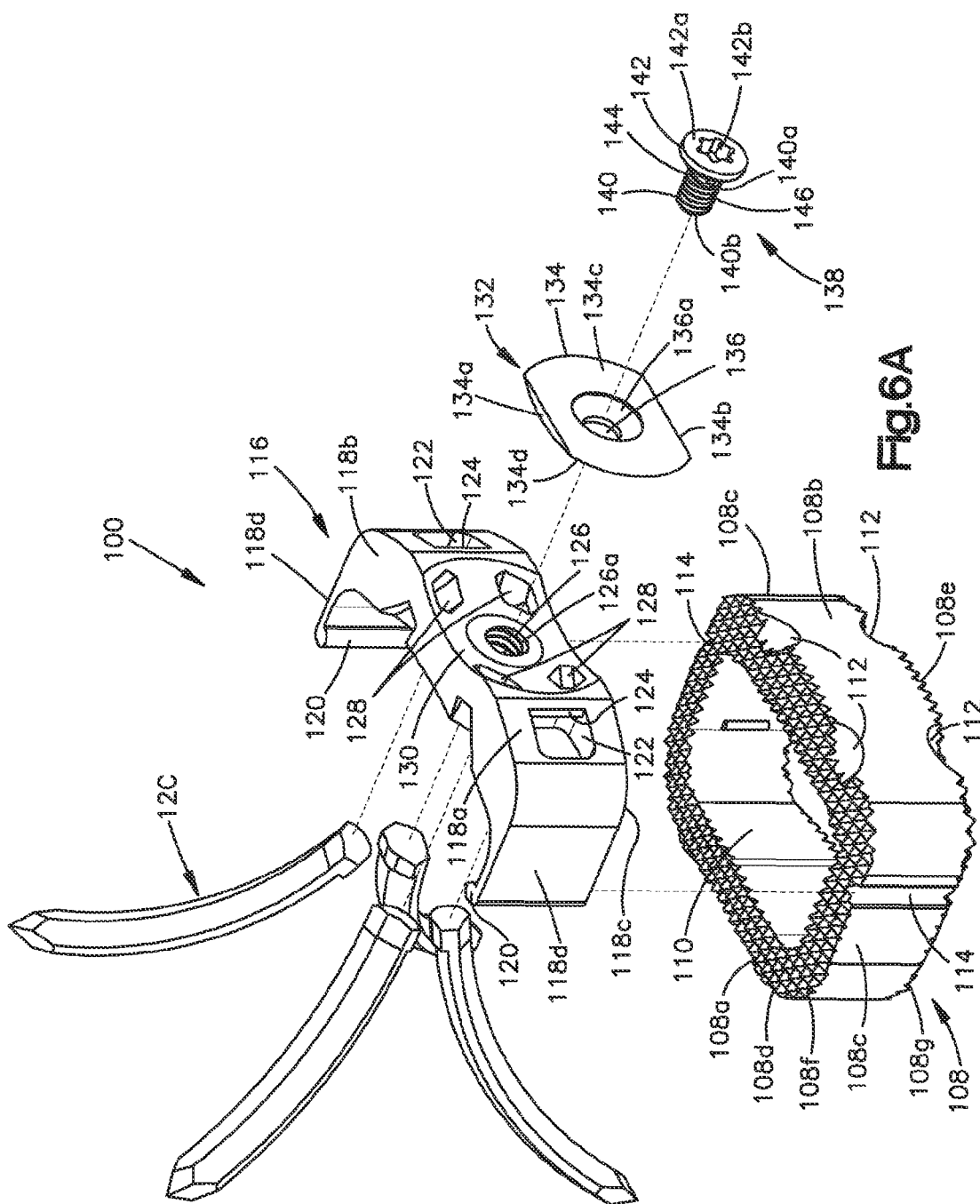


Fig. 4B



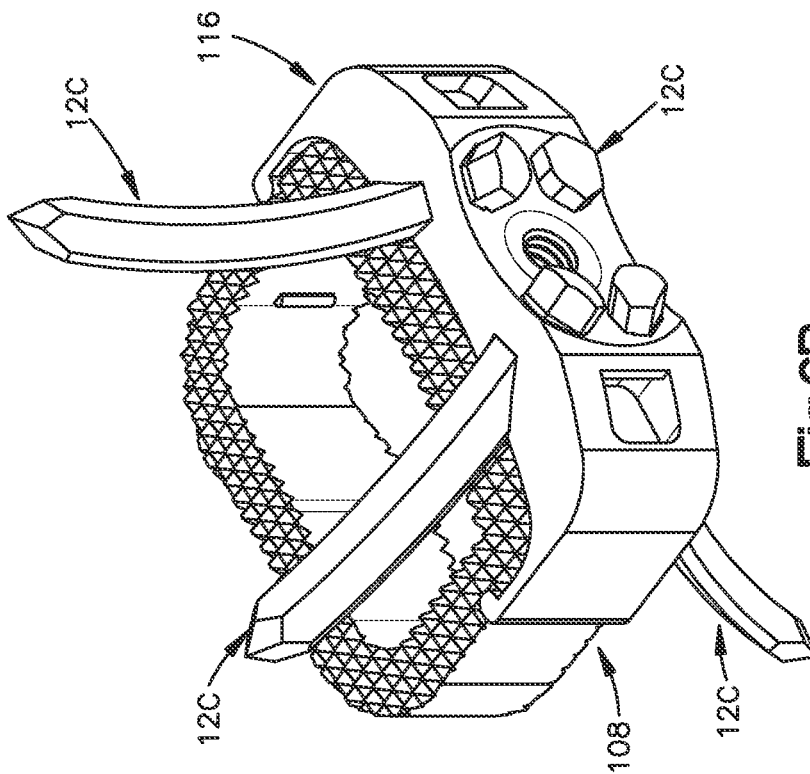


Fig. 6B

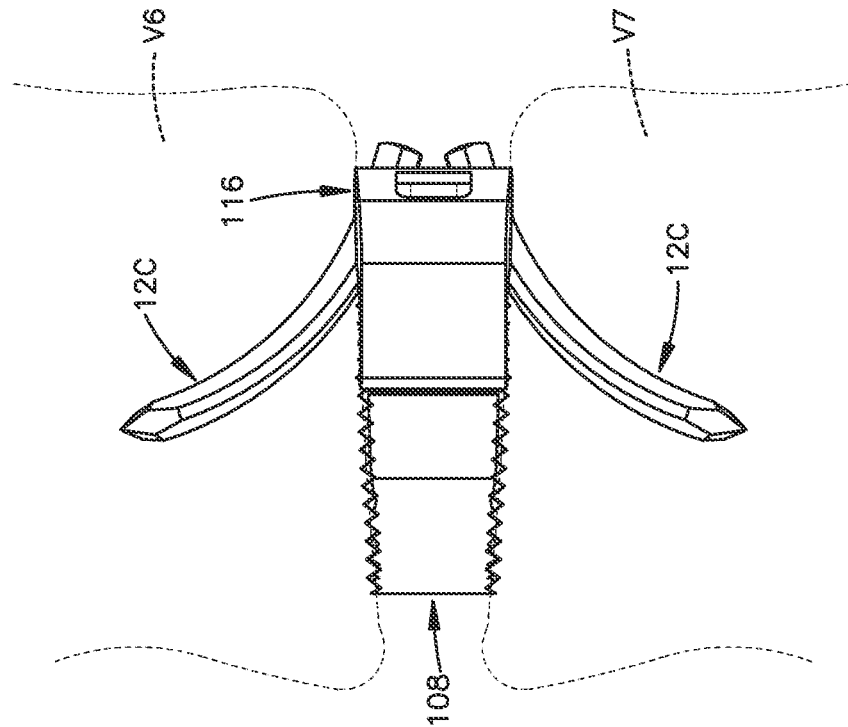
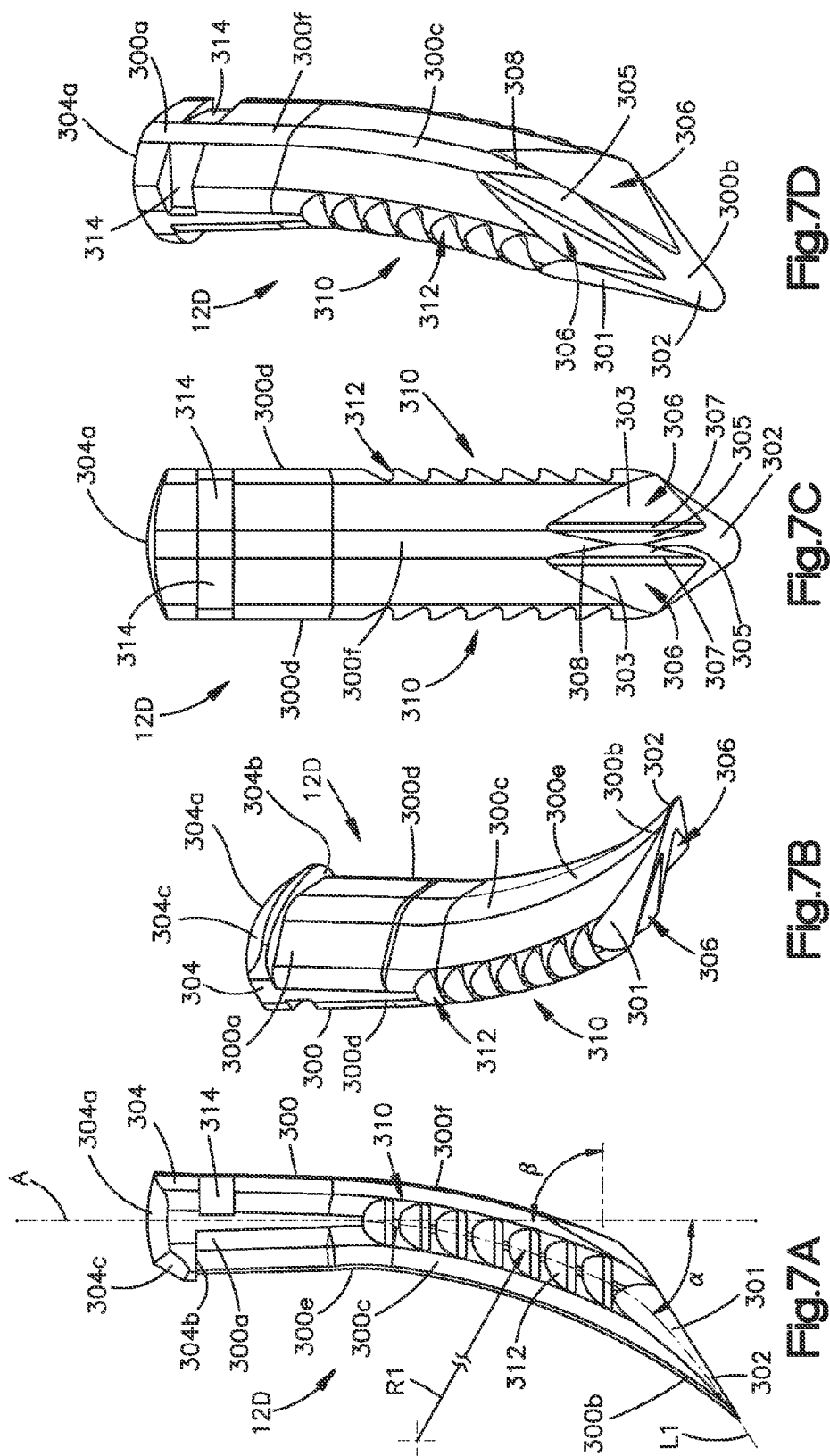
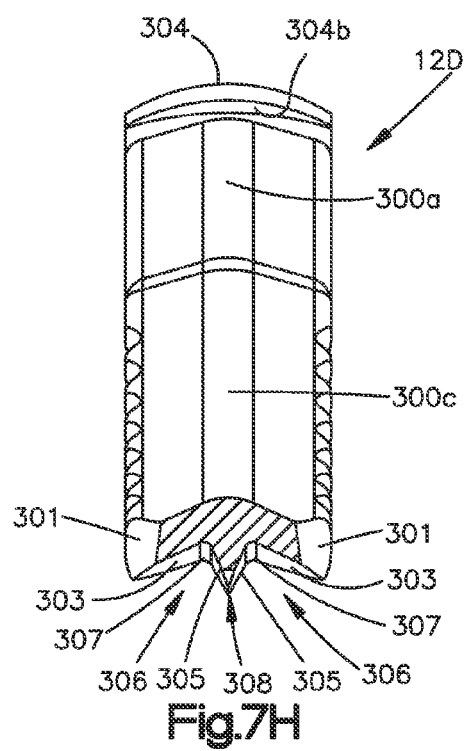
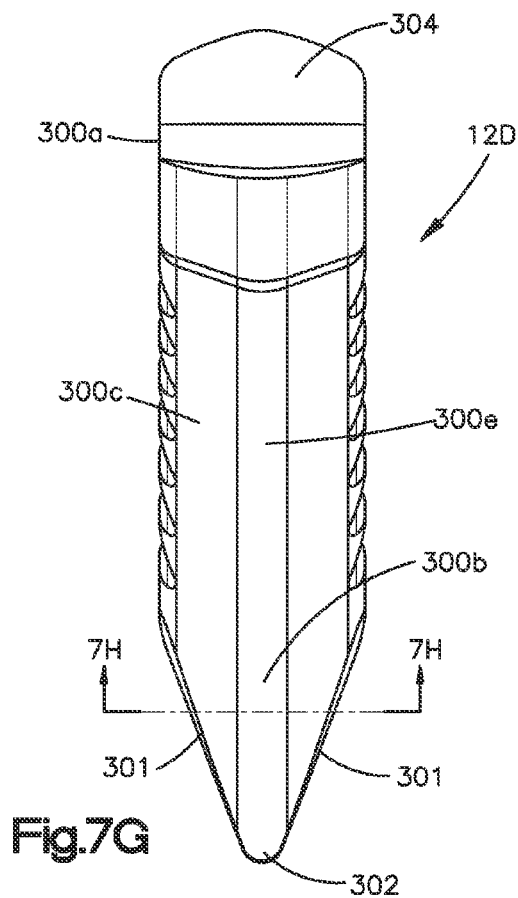
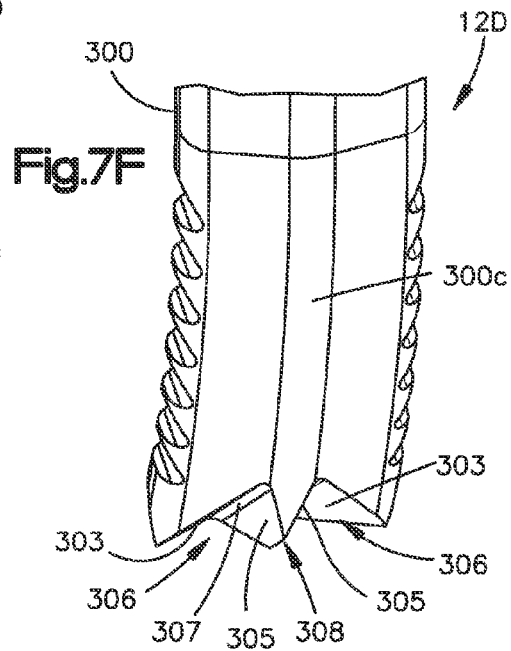
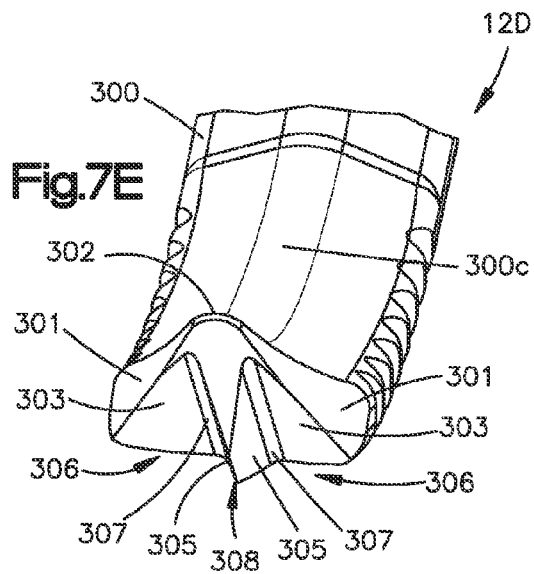


Fig. 6C





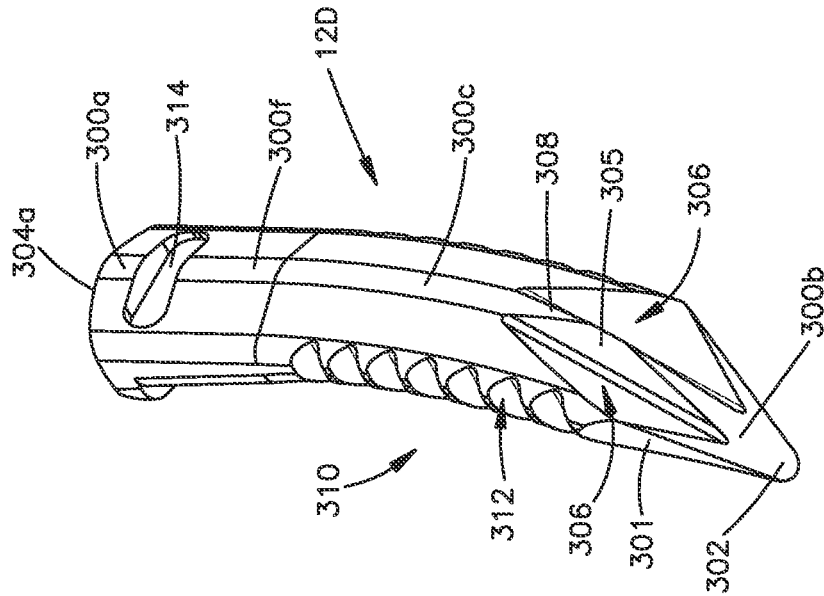


Fig. 7J

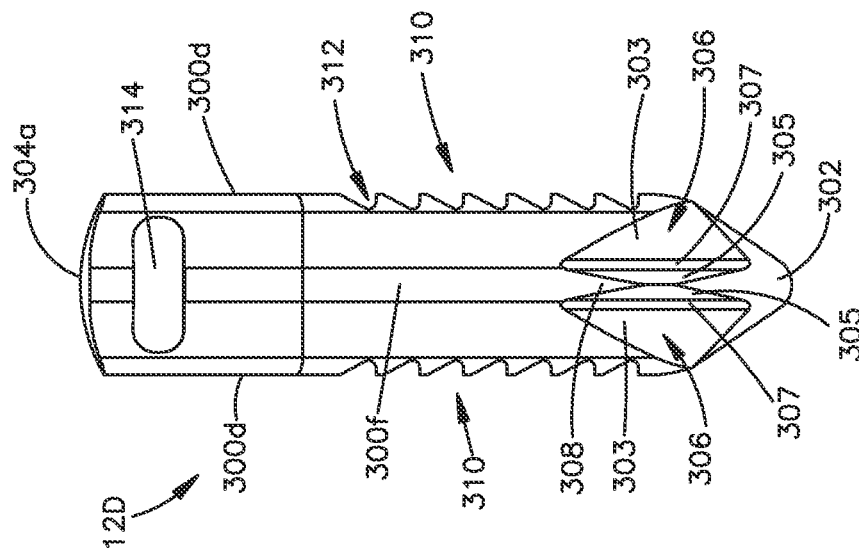
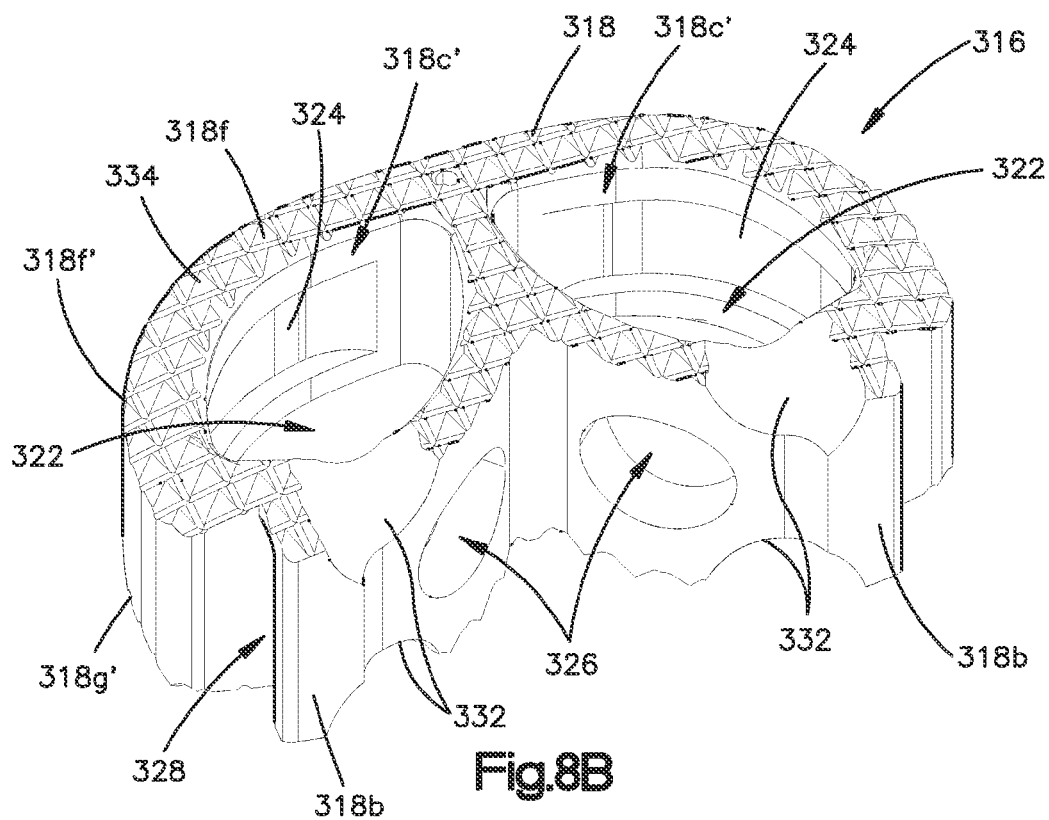
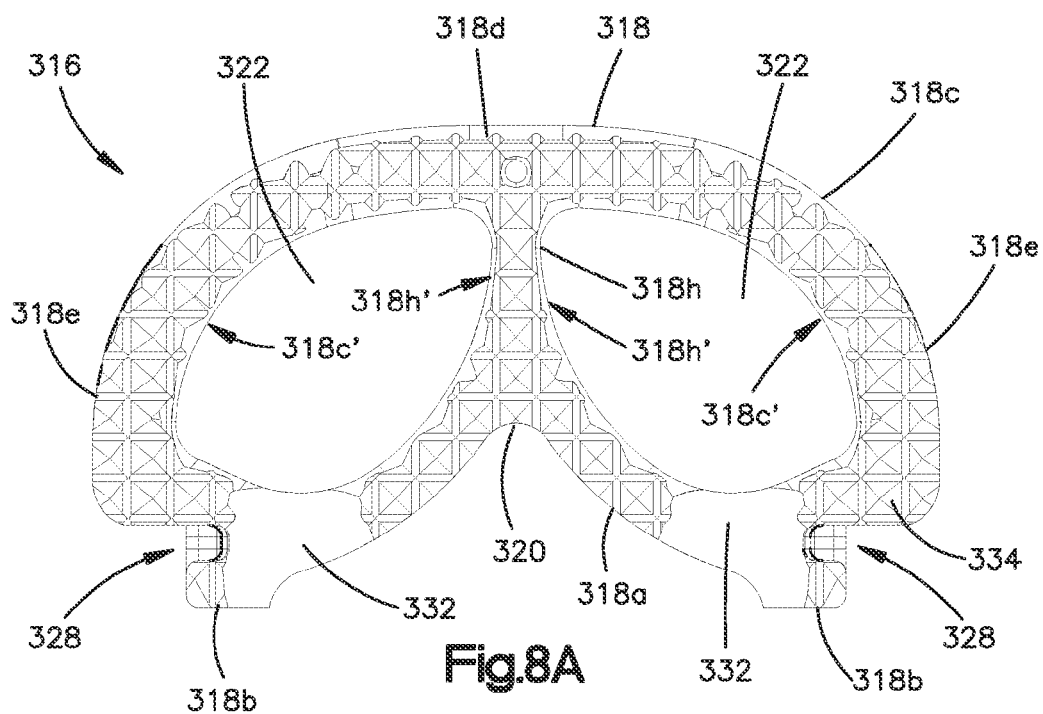


Fig. 7I



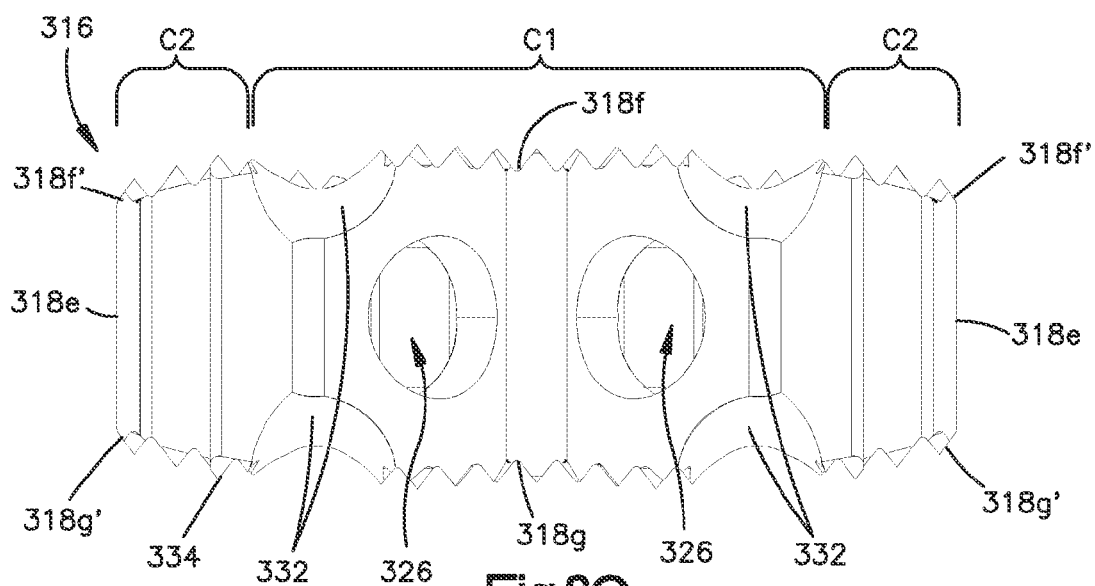


Fig. 8C

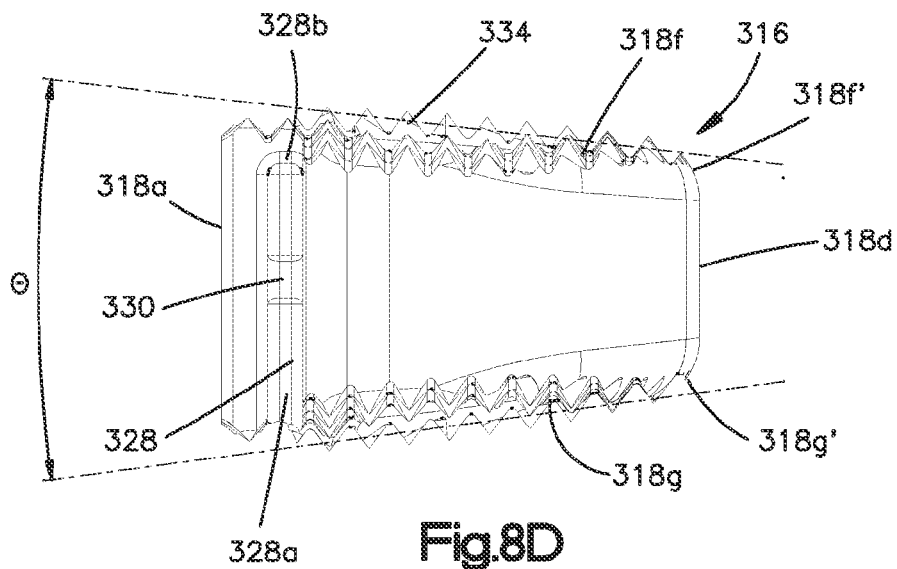
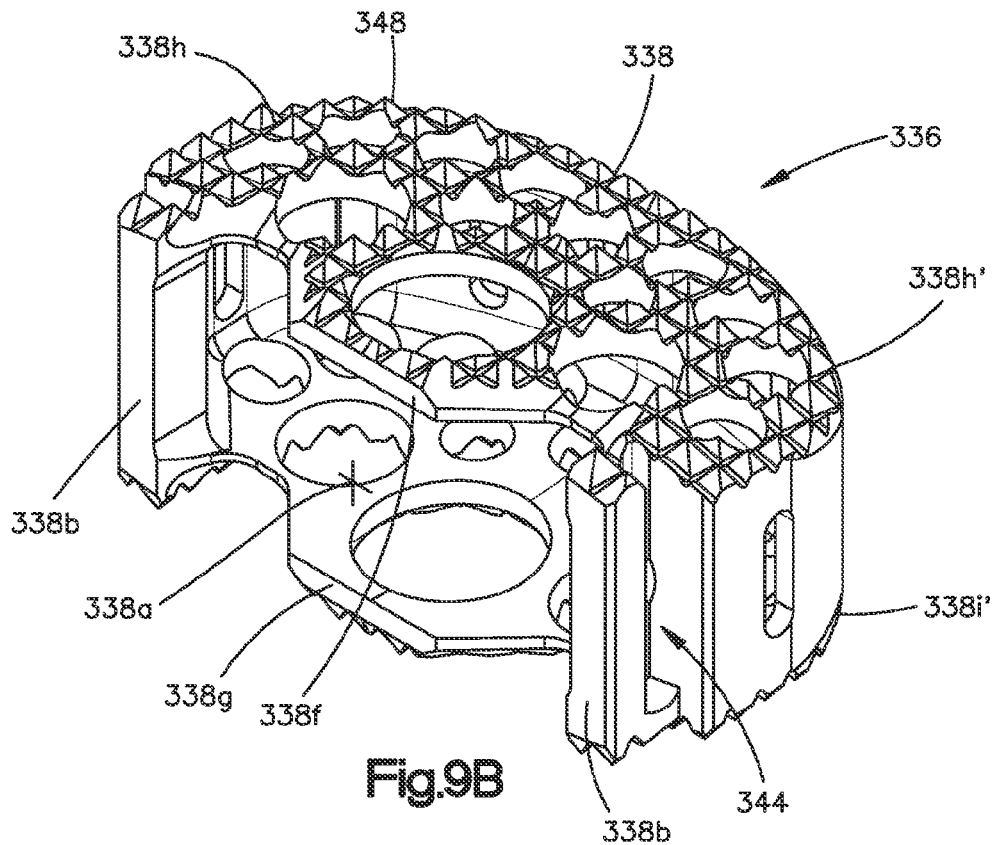
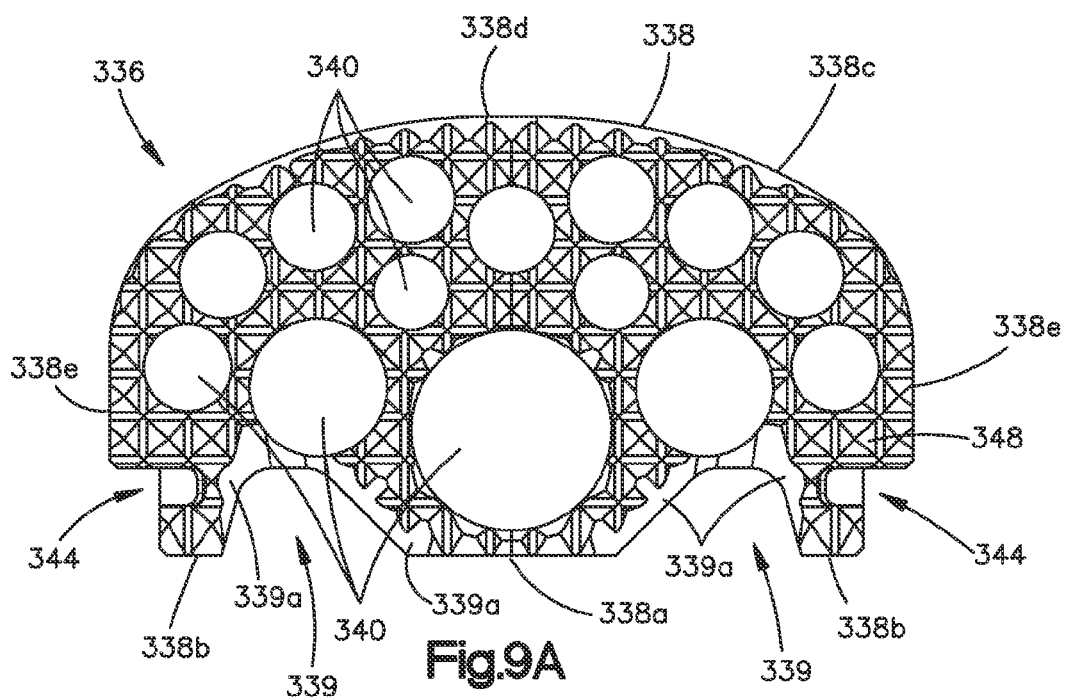


Fig. 8D



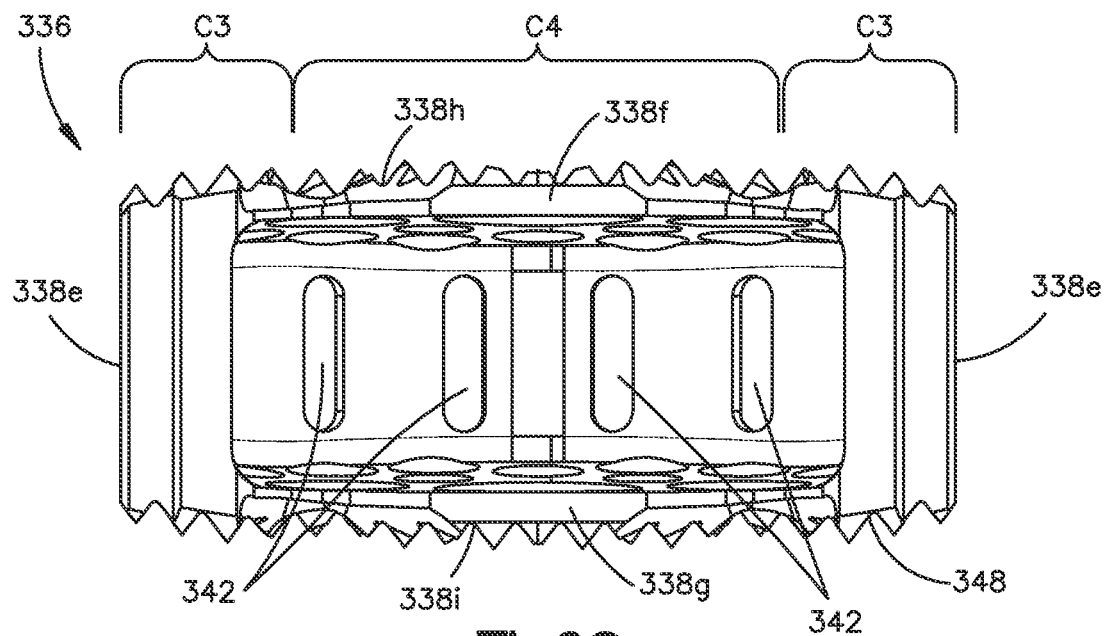


Fig.9C

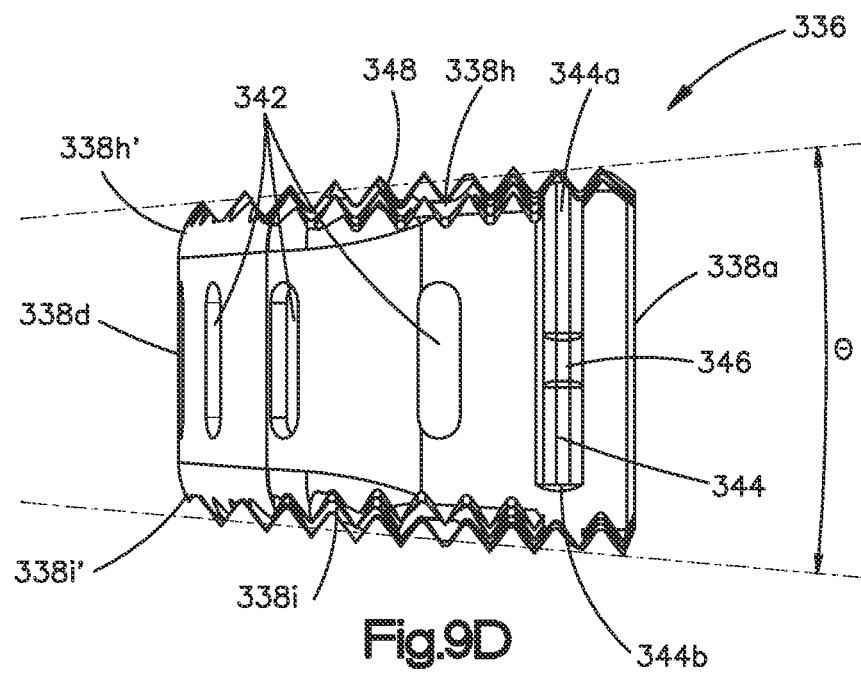
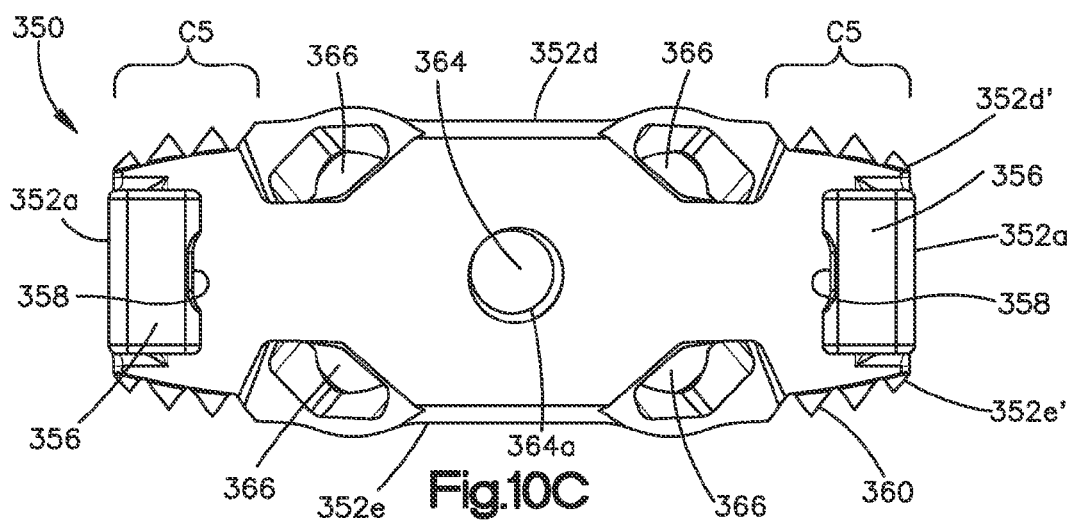
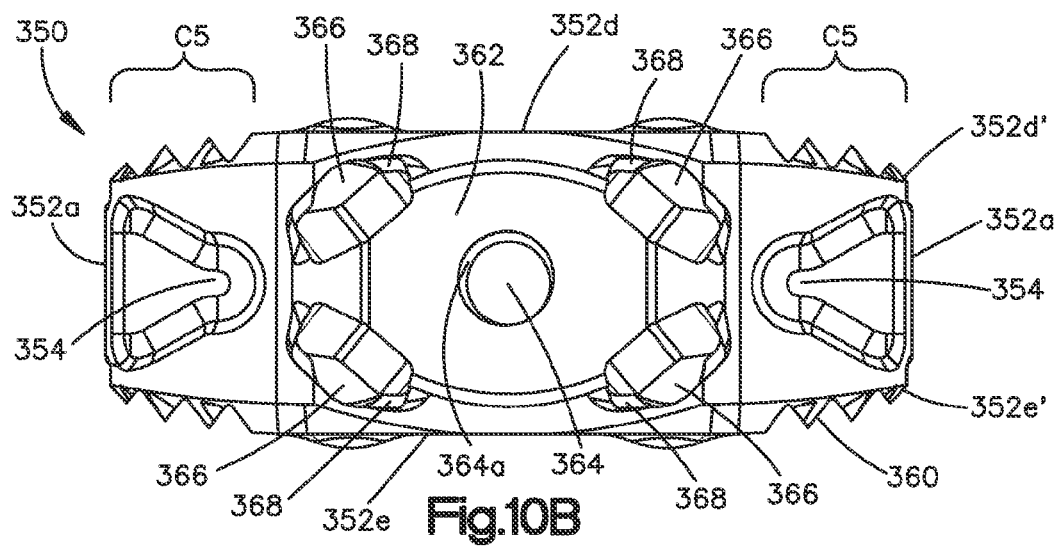
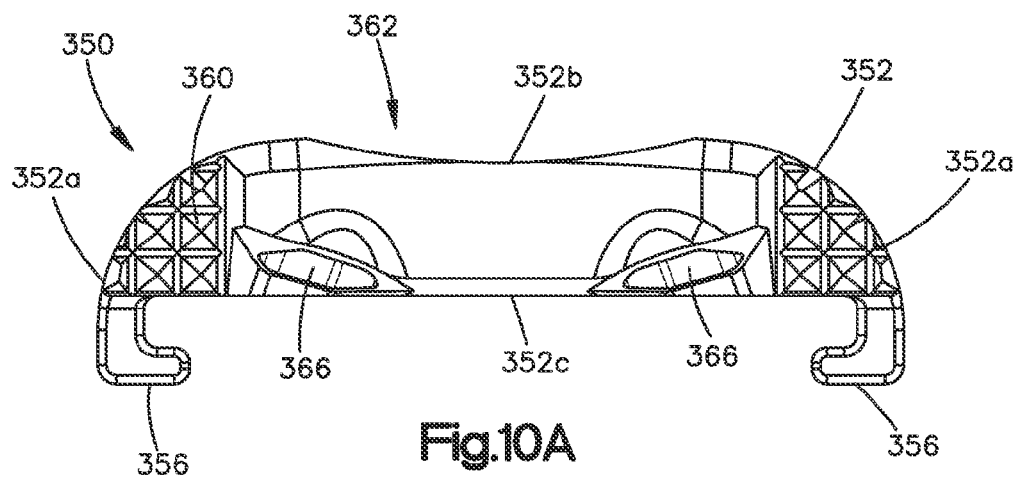
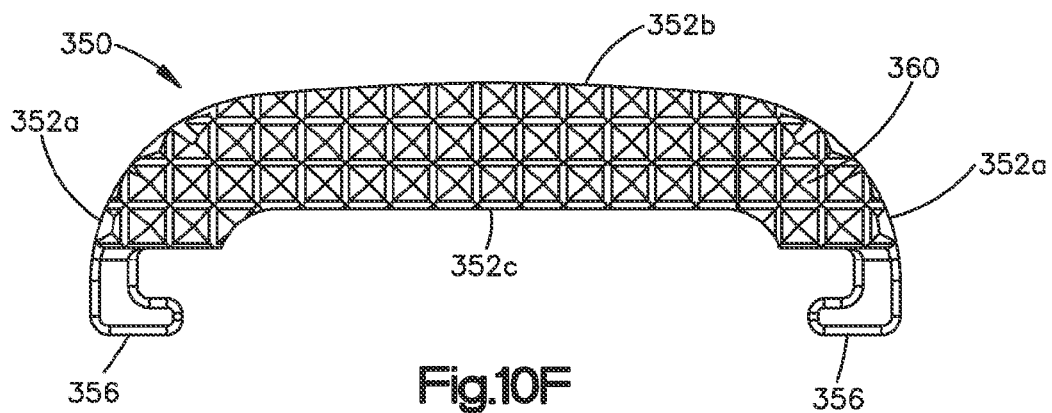
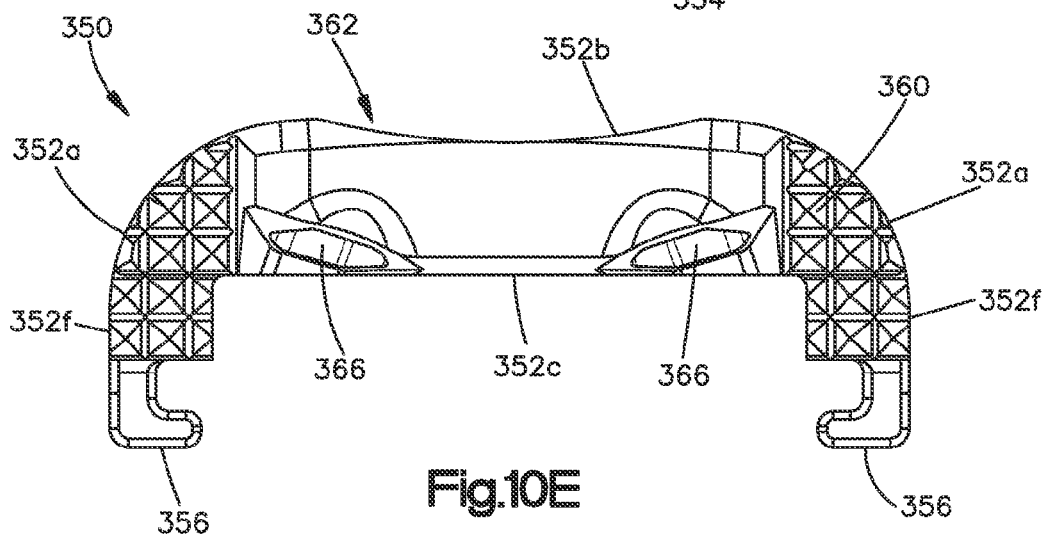
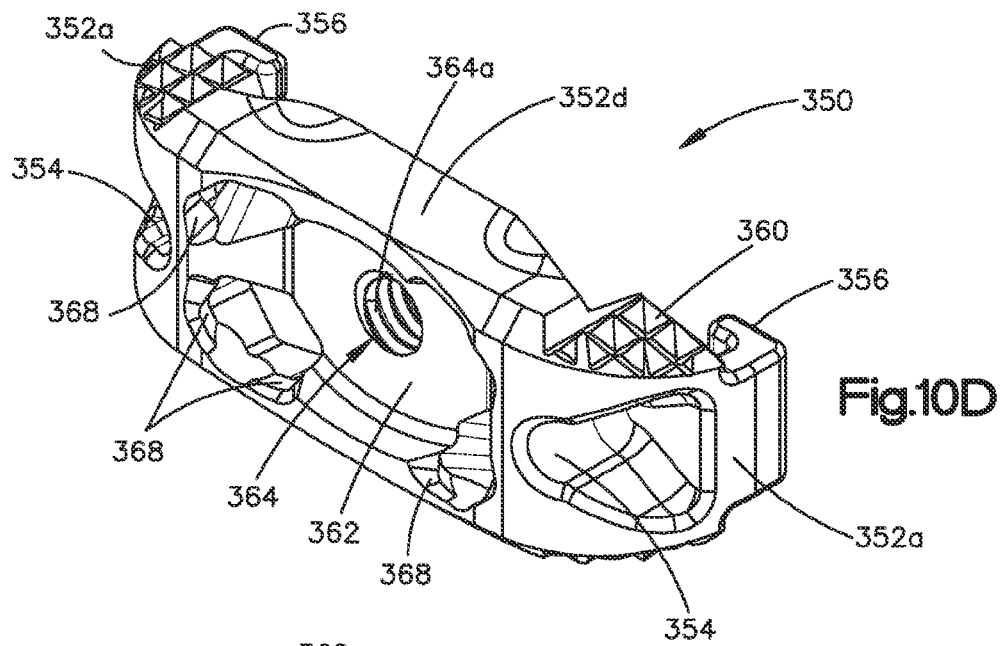


Fig.9D





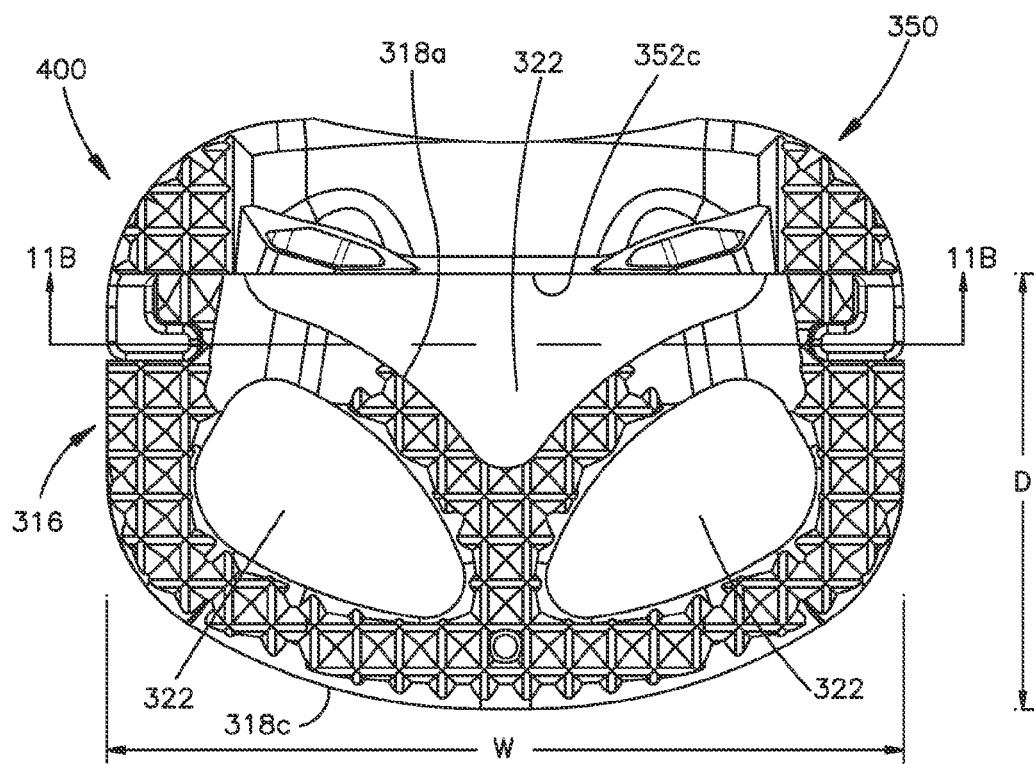


Fig.11A

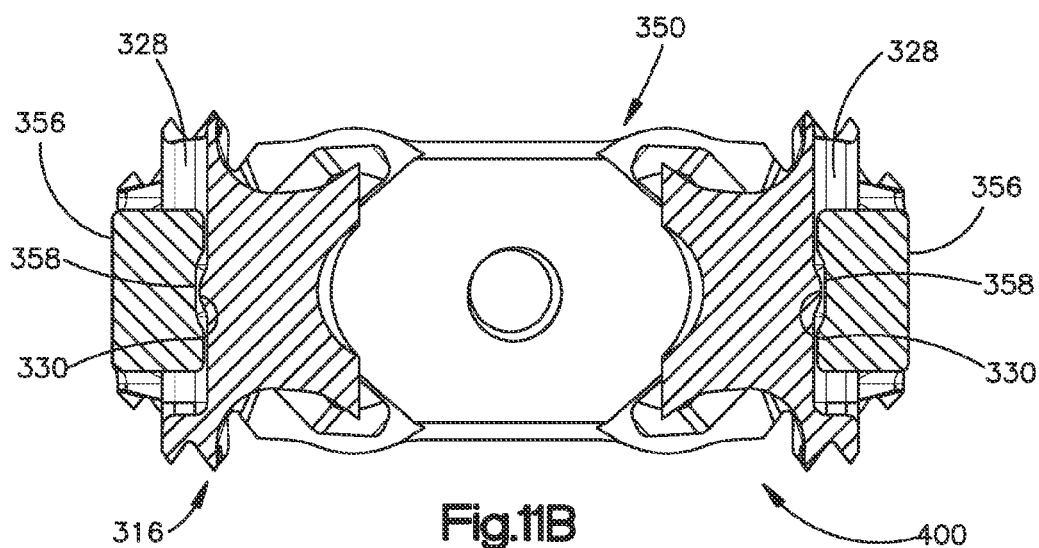
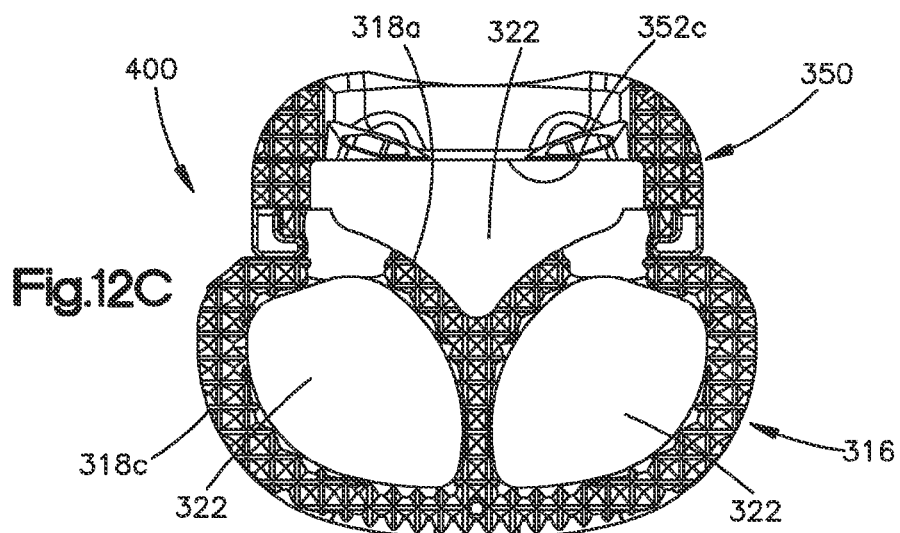
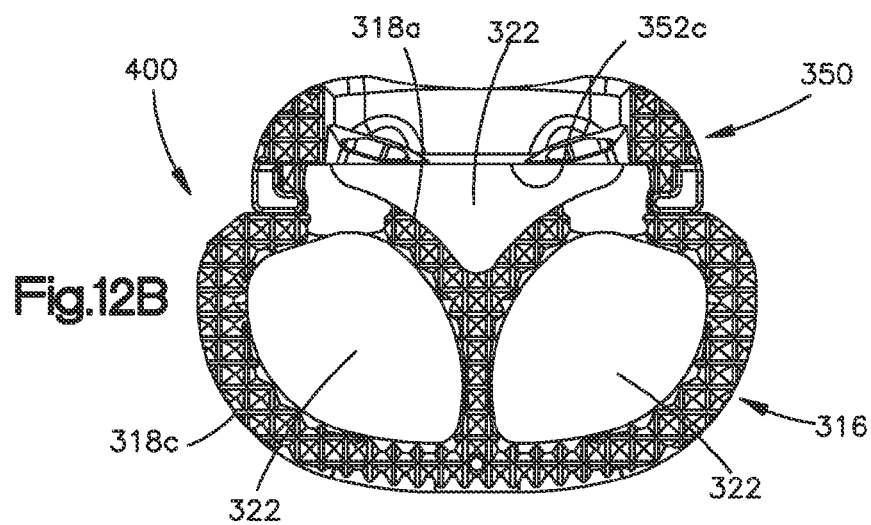
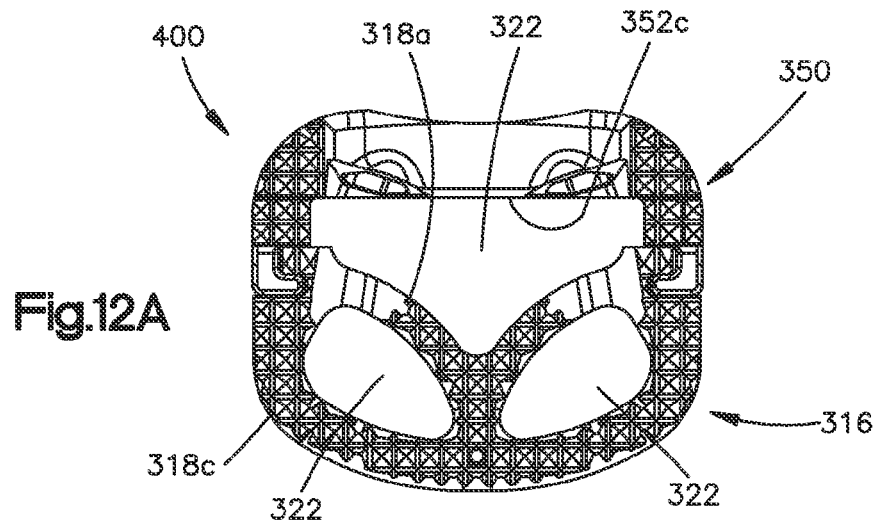
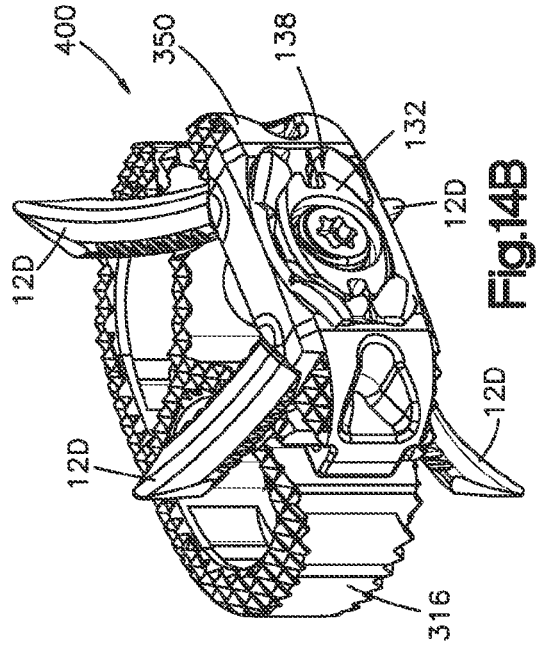
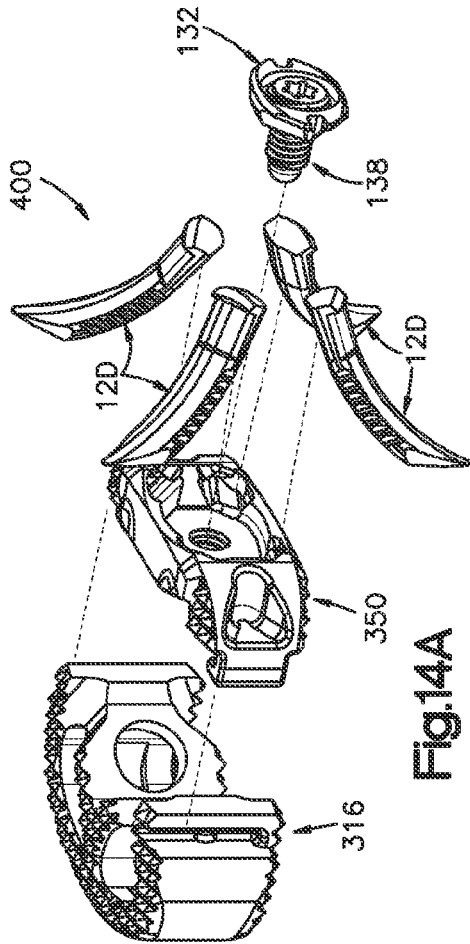
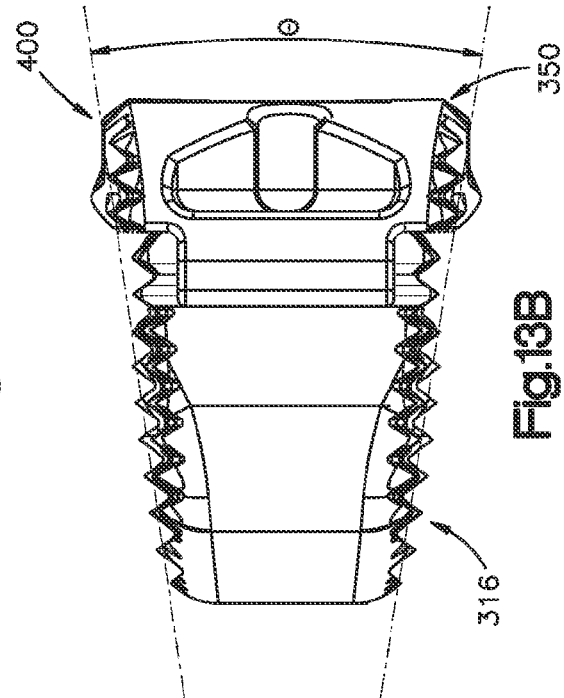
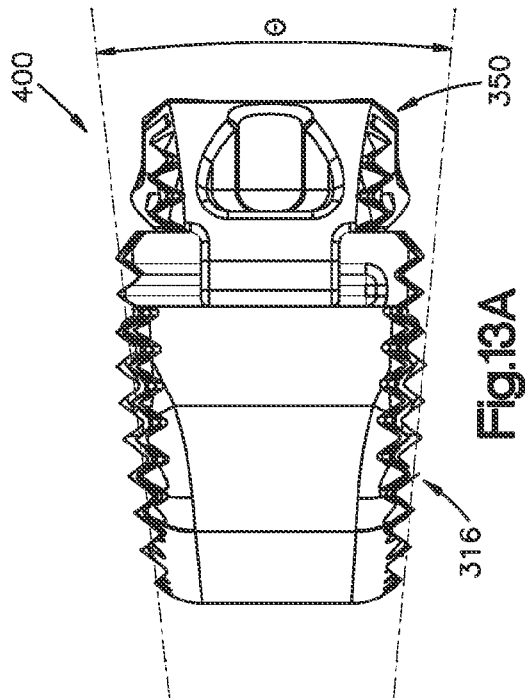


Fig.11B





1

ARCuate FIXATION MEMBER**CROSS-REFERENCE TO RELATED APPLICATIONS**

This patent application is a continuation of U.S. patent application Ser. No. 13/070,883, filed Mar. 24, 2011, which is a continuation-in-part of and claims priority to U.S. patent application Ser. No. 12/761,101, filed Apr. 15, 2010. U.S. patent application Ser. No. 12/761,101 claims priority to U.S. provisional patent application No. 61/169,461, filed Apr. 15, 2009. The disclosures of each application listed in this paragraph are hereby incorporated by reference as if set forth in their entireties herein.

TECHNICAL FIELD

The present disclosure relates generally to orthopedics, and in particular relates to fixation systems, intervertebral implants, and associated surgical methods and procedures for using same.

BACKGROUND

Spinal fixation systems such as pedicle screw and rod constructs are commonly used to promote fusion between intervertebral bodies. The insertion of pedicle screws typically requires a linear "line-of-approach" trajectory that is aligned with the longitudinal axis of the screw, in order to accommodate the access and delivery instruments. Similarly, anchors such as bone screws may be used to directly fix intervertebral implants to vertebral bodies, typically requiring the insertion of several screws at unique angles oblique to the sagittal and/or transverse plane, and thus multiple lines-of-approach. However, in a variety of surgical situations, achieving a desired trajectory for screw insertion can be difficult due to the patient's anatomy obstructing a linear line-of-approach. For example, medially-directed placement of pedicle screws into the sacrum is desirable to prevent screw loosening and/or pullout, but can be prohibited due to the iliac crest obstructing the linear line-of-approach.

SUMMARY

In accordance with one embodiment, a bone fixation member configured to be inserted in a vertebral body includes a fixation body having opposing proximal and distal ends and a curved intermediate portion extending between the proximal and distal ends. A tip configured to cut into bone is defined at the distal end. A guidance member is disposed at the tip and extends toward the proximal end of the body. The guidance member is configured to guide the tip along an insertion trajectory as the fixation member is inserted into a vertebral body.

The bone fixation member can be used with an intervertebral implant that includes a spacer body that is configured to be implanted into an intervertebral space. The spacer body has an outer wall that defines at least a first aperture extending into the spacer body. The intervertebral implant also includes an insert that defines a plate. The insert is configured to be coupled to the spacer body such that the insert and the outer wall of the spacer body define a second aperture therebetween.

An alternative intervertebral implant that can be used with the bone fixation member includes a spacer body that has upper and lower plates and an outer wall extending between

2

the upper and lower plates. The spacer body has a plurality of apertures extending through each of the upper and lower plates. The intervertebral implant also includes an insert that defines a plate. The insert is configured to be coupled to the spacer body such that the insert is disposed opposite at least a portion of the outer wall.

BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing summary, as well as the following detailed description of the preferred embodiments of the application, will be better understood when read in conjunction with the appended drawings. For the purposes of illustrating the arcuate fixation member and intervertebral implants for use therewith, there are shown in the drawings preferred embodiments. It should be understood, however, that the instant application is not limited to the precise arrangements and/or instrumentalities illustrated in the drawings, in which:

FIG. 1A is a side elevation view of an arcuate fixation member constructed in accordance with an embodiment;

FIG. 1B is a perspective view of the arcuate fixation member illustrated in FIG. 1A;

FIG. 2A is a top elevation view of an intervertebral implant spacer for use with arcuate fixation members, constructed in accordance with an embodiment;

FIG. 2B is a front elevation view of the intervertebral implant spacer illustrated in FIG. 2A;

FIG. 2C is a side elevation view of the intervertebral implant spacer illustrated in FIG. 2A;

FIG. 3A is a front elevation view of an insert plate for use with the intervertebral implant spacer illustrated in FIGS. 2A-C;

FIG. 3B is a top elevation view of the insert plate illustrated in FIG. 3A;

FIG. 4A is a front elevation view of a blocking plate for use with the insert plate illustrated in FIGS. 3A-B;

FIG. 4B is a top elevation view of the blocking plate illustrated in FIG. 4A;

FIG. 4C is a front elevation view of a blocking plate similar to the blocking plate illustrated in FIG. 4A, but constructed in accordance with an alternative embodiment;

FIG. 5 is a side elevation view of a locking screw for use with the insert plate and blocking plate illustrated in FIGS. 3A-B and 4A-B, respectively;

FIG. 6A is an exploded view of an intervertebral implant assembly constructed from the intervertebral implant system components illustrated in FIGS. 1A-5;

FIG. 6B is a perspective view of the intervertebral implant assembly illustrated in FIG. 6A, in an assembled configuration;

FIG. 6C is a side elevation view of the intervertebral implant assembly illustrated in FIG. 6B, inserted into an intervertebral space;

FIG. 7A is a side elevation view of an arcuate fixation member constructed in accordance with an alternative embodiment;

FIG. 7B is a front perspective view of the arcuate fixation member illustrated in FIG. 7A;

FIG. 7C is a rear elevation view of the arcuate fixation member illustrated in FIG. 7A;

FIG. 7D is a rear perspective view of the arcuate fixation member illustrated in FIG. 7A;

FIG. 7E is a front perspective view of a portion of the arcuate fixation member in FIG. 7A, showing a guidance member;

FIG. 7F is a rear perspective view of the portion of the arcuate fixation member in FIG. 7E;

FIG. 7G is a top elevation view of the arcuate fixation member illustrated in FIG. 7A;

FIG. 7H is a sectional front elevation view of the arcuate fixation member illustrated in FIG. 7G, taken along line 7H-7H;

FIG. 7I is a rear elevation view of an arcuate fixation member similar to the arcuate fixation member illustrated in FIG. 7A, but constructed in accordance with an alternative embodiment;

FIG. 7J is a rear perspective view of the arcuate fixation member illustrated in FIG. 7I;

FIG. 8A is a top elevation view of an intervertebral implant spacer for use with arcuate fixation members, constructed in accordance with an alternative embodiment;

FIG. 8B is a perspective view of the intervertebral implant spacer illustrated in FIG. 8A;

FIG. 8C is a front elevation view of the intervertebral implant spacer illustrated in FIG. 8A;

FIG. 8D is a side elevation view of the intervertebral implant spacer illustrated in FIG. 8A;

FIG. 9A is a top elevation view of an intervertebral implant spacer for use with arcuate fixation members, constructed in accordance with another alternative embodiment;

FIG. 9B is a perspective view of the intervertebral implant spacer illustrated in FIG. 9A;

FIG. 9C is a front elevation view of the intervertebral implant spacer illustrated in FIG. 9A;

FIG. 9D is a side elevation view of the intervertebral implant spacer illustrated in FIG. 9A;

FIG. 10A is a top elevation view of an insert plate for use with the intervertebral implant spacers illustrated in FIGS. 8A-D and 9A-D;

FIG. 10B is a front elevation view of the insert plate illustrated in FIG. 10A;

FIG. 10C is a rear elevation view of the insert plate illustrated in FIG. 10A;

FIG. 10D is a perspective view of the insert plate illustrated in FIG. 10A;

FIG. 10E is a top elevation view of the insert plate illustrated in FIG. 10A, constructed in accordance with an alternative embodiment;

FIG. 10F is a top elevation view of the insert plate illustrated in FIG. 10A, constructed in accordance with another alternative embodiment;

FIG. 11A is a top elevation view of an intervertebral implant constructed with an alternative embodiment of the intervertebral implant spacer illustrated in FIGS. 8A-D and the insert plate illustrated in FIGS. 10A-D;

FIG. 11B is a sectional elevation view of the intervertebral implant illustrated in FIG. 11A, taken along line 11B-11B;

FIG. 12A is a top elevation view of the intervertebral implant illustrated in FIG. 11A, constructed in accordance with an alternative embodiment;

FIG. 12B is a top elevation view of the intervertebral implant illustrated in FIG. 11A, constructed in accordance with another alternative embodiment;

FIG. 12C is a top elevation view of the intervertebral implant illustrated in FIG. 11A, constructed in accordance with still another alternative embodiment;

FIG. 13A is a side elevation view of an intervertebral implant constructed in accordance with an embodiment; and

FIG. 13B is a side elevation view of the intervertebral implant illustrated in FIG. 12A, constructed in accordance with another embodiment.

FIG. 14A is an exploded view of an intervertebral implant constructed from the intervertebral implant system components illustrated in FIGS. 7A-8D and 10A-D; and

FIG. 14B is a perspective view of the intervertebral implant illustrated in FIG. 14A, in an assembled configuration.

DETAILED DESCRIPTION OF ILLUSTRATIVE EMBODIMENTS

Certain terminology is used in the following description for convenience only and is not limiting. The words "right", "left", "top" and "bottom" designate directions in the drawings to which reference is made. The words "inwardly" and "outwardly" refer to directions toward and away from, respectively, the geometric center of the device and designated parts thereof. The words, "anterior", "posterior", "superior", "inferior", "lateral", "medial", "sagittal", "axial", "coronal," "cranial," "caudal" and related words and/or phrases designate preferred positions and orientations in the human body to which reference is made and are not meant to be limiting.

The words "arcuate" and "curved" as used herein refer generally to the varying physical geometry of an object along an axis coincident to the object, for example the deviation from straightness of the body of an arcuate fixation member along a central longitudinal axis defined within the body of the object between its proximal and distal ends. Generally, with reference to a straight axis projected from a first end of such an object, as distance from the first end of the object increases along the central longitudinal axis of the object, distance between the central longitudinal axis of the object and the straight axis increases more or less continuously, so that the body of the object defined along its central longitudinal axis takes on a curved or arcuate shape. The resulting curvature of the central longitudinal axis may exhibit a constant or uniform radius with respect to a point in space defined remotely from the body of the object. Alternatively, a non-uniform or varying radius of curvature may be defined. The curvature of the body of the object defined by the longitudinal axis may also vary in direction with respect to a Cartesian coordinate system. The curvature may be uniformly distributed along the body of the object, for example between the proximal and distal ends of the object, or may be localized within one or more distinct segments of the body of the object. The curvature of the object may be significantly smooth and continuous along its central longitudinal axis, may be defined by a series of straight interconnected segments where each successive segment defines an increasing angle between the central longitudinal axis of the body of the object and the straight axis, or any combination thereof.

The words "vertebral body" as used herein should be interpreted broadly to include all the bones and bony structures found within and in the immediate proximity of the human spinal system, including but not limited to those found in the cervical region, the thoracic region, the lumbar region, and the sacral curve region.

The terminology intended to be non-limiting includes the above-listed words, derivatives thereof and words of similar import.

Referring initially to FIGS. 1A-6C, example embodiments of components of an intervertebral implant system 100 comprising a bone fixation member which can define an arcuate fixation member 12C as illustrated, an intervertebral implant spacer 108, an insert plate 116, a blocking plate 132, and a locking screw 138 are illustrated. Applications of the

intervertebral implant system **100** could include, but are not limited to, fixation of the endplate components of a total disc replacement to vertebral bodies, direct fixation of an intervertebral implant to vertebral bodies, fixation into osteoporotic bone, and the like. The use of the systems and/or methods utilizing arcuate fixation members disclosed herein are particularly suitable when a linear line-of-approach for delivering a fixation member is undesirable. It should be noted that the physical characteristics of the arcuate fixation members disclosed herein may cause them to be alternately described as curved fixation members, arcuate or curved blades, arcuate or curved pins, arcuate or curved nails, or other terms of similar descriptive import.

As will become appreciated from the description below, one or more fixation members **12C** may be utilized to securely anchor an assembled configuration of intervertebral implant system **100** within an intervertebral space between adjacent vertebral bodies. Unless otherwise indicated, the intervertebral implant system **100** and its components can be manufactured from any suitable biocompatible material known in the art including but not limited to titanium, titanium alloy such as TAN, commercially pure titanium, stainless steel, tantalum, polymers such as polyether ether ketone (PEEK), reinforced plastics, allograft bone, and the like.

Referring now to FIGS. 1A-B, the arcuate fixation member **12C** includes a body **102** defining a proximal end **102a** and a distal end **102b** opposite the proximal end. The distal end **102b** may comprise a tip **104** configured to cut into underlying structure or bone. The body **102** may further define an intermediate portion between the proximal end **102a** and the distal end **102b** that is curved along a central curved axis L1. In an embodiment, the intermediate portion is curved along substantially the entire length of the body **102** between the proximal end **102a** and the distal end **102b**. Alternatively, one or more distinct portions of the intermediate portion between the proximal end **102a** and the distal end **102b** may be curved (not shown).

In the illustrated embodiment, the intermediate portion is curved along the central curved axis L1 in accordance with a uniform radius of curvature R1. Alternatively, the intermediate portion may define a non-uniform radius of curvature along the central curved axis L1. In a preferred embodiment, the curvature of the intermediate portion may be smooth and continuous. Alternatively, the curvature of the intermediate portion may be defined by a series of substantially straight sections (not shown), with each substantially straight section aligned along an individual longitudinal axis corresponding to the individual section, where the magnitude of an angle α with respect to a perpendicular reference axis extended from the proximal end **102a** increases in magnitude with the distance of each subsequent straight section from the proximal end **102a**.

The arcuate fixation member **12C** may have a head **106** defined at the proximal end **102a** of the body **102**. The head **106** may extend radially outward from the proximal end **102a** of the body **102** in a direction perpendicular to the longitudinal axis L1. In an example embodiment, the head **106** may extend from the body **102** in a direction generally opposite from the direction of curvature of the body **102**, as depicted in FIGS. 1A-B. In alternative embodiments, the head **106** may extend from the body **102** in a direction generally towards the direction of curvature of the body **102**. The head may define an upper surface **106a** configured for multi-angular engagement with a complementary surface of a delivery instrument, and a lower surface **106b** opposite the upper surface **106a** and configured to engage another com-

ponent of the intervertebral implant system **100**, for example the insert plate **116**, when the arcuate fixation member **12C** is in a fully inserted position.

Referring now to FIGS. 2A-C, the intervertebral implant spacer, or spacer **108** is defined by a posterior side **108a**, an anterior side **108b** opposite the posterior side, lateral sides **108c**, an upper surface **108d**, and a lower surface **108e** opposite the upper surface. In an example embodiment, a portion of the posterior side **108a** between the lateral sides **108c** may be curved inwardly in the direction of the anterior side **108b**, defining a rounded, generally rectangular kidney-like footprint, as depicted in FIG. 2A. In an alternative embodiment, a portion of the posterior side **108a** between the lateral sides **108c** may be curved outwardly in a direction away from the anterior side **108b** (not shown). In another alternative embodiment, the posterior side **108a** may be substantially straight between the lateral sides **108c**, defining a rounded, generally rectangular footprint (not shown). The spacer **108** may have a central bore **110** defined there-through, the shape of which substantially conforms to the footprint of the spacer **108** (e.g., a rounded, generally rectangular kidney-like footprint, or a rounded, generally rectangular footprint, depending upon the geometry of the posterior side **108a**). The central bore **110** can be filled with bone growth inducing substances to allow bony ingrowth and to assist in fusion between the spacer **108** and adjacent vertebral bodies.

In an example embodiment of the spacer **108**, the upper and lower surfaces **108d** and **108e** may have gripping structures **108h** such as teeth, spikes, or similar structures, defined thereon and configured to facilitate gripping engagement between the upper and lower surfaces **108d** and **108e** and the end plates of adjacent vertebral bodies. The teeth **112** may be pyramidal, saw toothed or other similar shapes. In alternative embodiments of the spacer **108**, portions of and/or the entirety of the upper and lower surfaces **108d** and **108e** may be substantially smooth and devoid of any protrusions. Upper and lower edges **108f** and **108g**, defined where the upper and lower surfaces **108d** and **108e** intersect with the posterior, anterior, and lateral sides **108a**, **108b**, and **108c** respectively around the outer perimeter of the spacer **108**, may be rounded (not shown). In an example embodiment, the upper and lower edges **108f** and **108g** may be rounded using a uniform radius of curvature around the perimeter of the implant. In an alternative embodiment, the upper and lower edges **108f** and **108g** may be rounded using a non-uniform radius of curvature around the perimeter of the implant. In another alternative embodiment, the upper and lower edges **108f** and **108g** along the anterior side **108b** may be rounded with a greater radius than the remainder of the upper and lower edges **108f** and **108g**, such that a bull nose outer surface (not shown) is created on the anterior side **108b** of the implant. Rounding upper and lower edges **108f** and **108g** may facilitate easier insertion of the spacer **108**, for example by minimizing required distraction of the end plates of adjacent vertebral bodies.

In an example embodiment, the spacer **108** has a generally wedge-shaped side-view profile. As illustrated in FIG. 2C, this wedge shape is defined by a gradual decrease in the height of the spacer **108** (as measured between the upper and lower surfaces **108d** and **108e**) extending between the posterior side **108a** in the direction of the anterior side **108b**. The spacer **108** has a generally constant height between lateral sides **108c**. In alternative embodiments, the spacer **108** may have a gradual increase in height followed by a gradual decrease in height extending from one lateral side **108c** to the other, and/or may have a generally constant

7

height between the posterior and anterior sides **108a** and **108b**, or may have convex and/or concave upper and lower surfaces **108d** and **108e**, thereby defining a gradual increase in height followed by a gradual decrease in height extending from the posterior side **108a** to the anterior side **108b** and from one lateral side **108c** to the other.

A plurality of grooves **112** may be defined on the spacer **108** where the upper and lower surfaces **108d** and **108e** intersect with the anterior side **108b**. The grooves **112** may be concave and may be configured to align with arcuate grooves **128** of the insert plate **116** when the spacer **108** and the insert plate **116** are in an assembled configuration. In an example embodiment, the grooves **112** may be substantially smooth and devoid of any protrusions. Retaining grooves **114** may be defined within the lateral sides **108c** of the spacer **108** between the upper and lower surfaces **108d** and **108e**. The retaining grooves **114** may be configured to releasably engage complementary engaging ribs **120** of the insert plate **116**.

Referring now to FIGS. 3A-B, the fixation plate, or insert plate, or insert **116** is defined by a generally C-shaped, channel-like body **118** that includes an anterior side **118a** with upper and lower sides **118b** and **118c** opposite each other, and lateral sides **118d** extending from opposite sides of the anterior side **118a** in a generally perpendicular direction from the anterior side **118a**. The anterior, upper, lower, and lateral sides **118a**, **118b**, **118c**, and **118d** may form a generally channel-like structure (in essence, a cradle) which may be configured to receive the anterior side **108b** and at least a portion of the lateral sides **108c** in partial nested engagement. As such, the upper and lower sides **108b** and **108c** may define gradual increases and/or decreases in height in a posterior direction from the anterior side **118a** and/or between the lateral sides **108d**, in order to generally conform the insert plate **116** to the geometry of the spacer **108**. The lateral sides **118d** may have engaging ribs **120** defined thereon at the ends opposite the anterior side **118a**, the engaging ribs **120** configured to be releasably received within the retaining grooves **114** of the spacer **108**.

The anterior side **118a** of the insert plate **116** may have a pair of apertures **122** defined therethrough configured to receive grasping members of a delivery instrument. In an example embodiment, the apertures **122** may be D-shaped, as illustrated in FIG. 3A. However any other aperture shape may be defined as appropriate. The apertures **122** may have a retaining rib **124** defined therein configured to engage with a complementary grasping rib of the delivery instrument. The anterior side **118a** of the insert plate **116** may also have a central bore **126** defined therethrough having an inner surface **126a** with threads configured to engage complementary threads of a locking screw **138**. The anterior side **118a** of the insert plate **116** may also have a concave recess **130** defined therein configured to receive a complementary convex surface **134d** of the blocking plate **132**.

The anterior side **118a** of the insert plate **116** may also have a plurality of arcuate grooves **128** defined therethrough configured to slidably receive the arcuate fixation members **12C** and to define an insertion trajectory for each of the arcuate fixation members **12C**. In an example embodiment, the arcuate grooves **128** may have a generally uniform cross sectional geometry configured to closely conform to the cross sectional geometry of the body **102** of the arcuate fixation member **12C** between the head **106** and the distal end **102b**. When an arcuate fixation member **12C** is in a fully inserted position within a respective arcuate groove **128**, the lower surface **106b** of the head **106** will be engaged with the outer surface of the anterior side **118a** of the insert plate **116**.

8

Because the upper surface **106a** of the head **106** will not be flush with the outer surface of the anterior side **118a** of the insert plate **116** in this configuration, it may be desirable to omit the blocking plate **132** and the locking screw **138**. In an alternative embodiment, the arcuate grooves **128** have a recessed ledge defined therein in the area where the arcuate grooves **128** intersect with the outer surface of the anterior side **118a** of the insert plate **116**, the recessed ledge being configured to receive the lower surface **106b** of the head **106** when the arcuate fixation member **12C** is in a fully inserted position, such that the upper surface **106a** of the head **106** is substantially flush with the outer surface of the anterior side **118a** of the insert plate **116**.

The arcuate grooves **128** may be disposed about the central bore **126** in any desired configuration and may define any insertion trajectories as appropriate. In the example embodiment depicted in FIGS. 3A-B, the arcuate grooves **128** are defined in opposing quadrants around the central bore **126**, with two arcuate grooves **128** located near the upper side **118b** and defining two generally cranial insertion trajectories, and two arcuate grooves **128** located near the lower side **118c** and defining two generally caudal insertion trajectories. It should be noted that this configuration of arcuate groove **128** locations and arcuate fixation member **12C** insertion trajectories is merely an example, and the scope of the instant disclosure should not be limited thereto.

Referring now to FIGS. 4A-B, the blocking plate **132** is defined by a generally disc-shaped body **134** with upper and lower surfaces **134a** and **134b** that can be planar as illustrated, an anterior surface **134c**, and a posterior surface **134d**. The disc-shaped body **134** can further define opposed side surfaces **135a** and **135b**, which can be convexly curved, extending between the upper and lower surfaces **134a-b**. The upper and lower surfaces **134a** and **134b** and the height of the body **134** (as measured between the upper and lower surfaces **134a** and **134b**) may be defined to match the height (as measured between the upper and lower surfaces **118b** and **118c**) of the anterior side **118a** of the insert plate **116** when the blocking plate **132** is in a fully assembled configuration. The anterior surface **134c** of the body **134** may be generally planar, or may be defined to match the outer surface of the anterior side **118a** of the insert plate **116** when the blocking plate **132** is in a fully assembled configuration. The posterior surface **134d** may be defined as a convex surface configured to engage with the concave recess **130** of the insert plate **116** when the blocking plate **132** is in a fully assembled configuration.

The posterior surface **134d** can also be configured to engage the heads **106** of the arcuate fixation members **12C** inserted into the arcuate grooves **128** of the insert plate **116**. For example, the posterior surface **134d** can operate to drive the arcuate fixation members **12C** into a fully inserted position within the insert plate **116** as the locking screw **138** is tightened. In addition to driving the arcuate fixation members **12C** into a fully inserted position, the blocking plate **138** can additionally prevent backout of the arcuate fixation members **12C**. It should be appreciated that the posterior surface **134d** of the blocking plate **132** is not limited to the illustrated convex surface, and that the posterior surface **134d** can define alternative geometries. For example, the posterior surface **134d** may define a plurality of angled surfaces, such as four angled surfaces in opposed quadrants of the posterior surface **134d**, each of the angled surfaces configured to engage with the head **106** of a corresponding arcuate fixation member **12C**.

The body **134** may have an aperture **136** defined there-through. In an example embodiment, the diameter of the

aperture 136 may be slightly larger than the diameter of the central bore 126 of the insert plate 116, such that a locking screw 138 may be inserted into the aperture 136 with no interference therebetween. In another embodiment, the diameter of the aperture 136 may be substantially the same as that of the central bore 126, and the inner surface of the aperture 136 may have threads defined thereon, the threads configured to engage complementary threads of the locking screw 138. The aperture 136 may further be defined by a concave recess 136a defined within the anterior surface 134c, the concave recess 136a configured to receive the convex head 142 of the locking screw 138.

It should be appreciated that the blocking plate 132 can be geometrically configured as desired so as to be received and nest in the concave recess 362 and coupled to the insert plate 350. For instance, referring to FIG. 4C, the upper and lower surfaces 134a-b of the disc-shaped body 134 can be curved, and bow outwards in accordance with one embodiment. Furthermore, the side surfaces 135a-b can extend substantially straight between the upper and lower surfaces 134a-b. The disc-shaped body 134 can further define beveled surfaces 137a-d that are connected between respective side surfaces 135a and 135b and respective upper and lower surfaces 134a and 134b. Pockets 139 a-b can be defined extending into the side surfaces 135 a-b, the pockets 139a-b configured to receive a driving instrument that braces against the blocking plate 132 so as to drive the locking screw 138 into the insert plate 350.

Referring now to FIG. 5, the locking screw 138 includes a shaft 140 that defines longitudinally opposing proximal and distal ends 140a and 140b, respectively, and a head 142 coupled to the proximal end 140a of the shaft 140, either directly or indirectly via an unthreaded neck 144 that is coupled between the proximal end 140a of the shaft 140 and the head 142. The head 142 can define a generally convex shape between the interface of the head 142 and the neck 144 that extends outward towards a proximal end 142a of the head 142. The convex shape of the head may be configured to engage the concave recess 136a of the blocking plate 132. Of course, the head 142 can assume any other suitable alternative shape as appropriate. Helical threads 146 extend radially out from the shaft 140 at locations at and between the proximal and distal ends 140a and 140b that are configured to engage complementary threads on the inner surface 126a of the central bore 126 of the insert plate 116. Thus, a substantial entirety of the shaft 140 between the proximal and distal ends 140a and 140b may be threaded. The distal end 142a of the head 142 may have driving members 142b defined therein, designed to engage with complementary driving members of a delivery instrument. It should be appreciated that the locking screw 138 can alternatively be provided in combination with the blocking plate 132 as a captive locking screw, wherein the locking screw 138 is rotatably retained within the aperture 136 of the blocking plate 132. It should be appreciated that the head 142 can be externally threaded.

Referring now to FIGS. 6A-C, an example embodiment of the intervertebral implant system 100 is illustrated in an exploded view and in a nearly completely assembled configuration. FIG. 6B depicts the intervertebral implant system 100 partially assembled outside of an intervertebral space (the blocking plate 132 and locking screw 138 have been omitted for simplicity). The spacer 108 has been seated within the insert plate 116 such that the retaining ribs are seated with the retaining grooves 114 on the lateral sides of the spacer 108. Four arcuate fixation members 12C have been inserted through corresponding arcuate grooves 128

within the insert plate 116, and have been driven to an almost fully inserted position. In a final assembled configuration, the arcuate fixation members 12C would be driven into their fully inserted position, the blocking plate 132 would be received within the concave recess 130 in the anterior side of the insert plate 116, and the locking screw 138 would be driven into the central bore 126 of the insert plate 116 and finally tightened, thereby blocking the arcuate fixation members 12C from backing out of the assembled intervertebral implant system 100.

FIG. 6C depicts an example embodiment of the intervertebral implant system 100 partially assembled inside of an intervertebral space between adjacent vertebral bodies V6 and V7 (the blocking plate and locking screw have been omitted for simplicity). As an initial step, the spacer 108 has been prepared for insertion, for example by being packed with bone growth inducing substance and/or having its outer surfaces properly prepared, and has been seated within the insert plate 116 such the retaining ribs are seated with the retaining grooves on the lateral sides of the spacer 108. The spacer 108 was then inserted into the intervertebral space between the adjacent vertebral bodies V6 and V7 using a delivery instrument (not shown). The delivery instrument was then used to deliver the four arcuate fixation members 12C into the arcuate grooves in the fixation plate 116 and drive them into an almost fully inserted position. During the final steps of the assembly process, the delivery instrument would be used to drive the arcuate fixation members 12C into their fully inserted position, the blocking plate would be received within the concave recess in the anterior side of the insert plate 116, and the locking screw would be driven into the central bore of the insert plate 116 and finally tightened, thereby blocking the arcuate fixation members 12C from backing out of the assembled intervertebral implant system 100.

Now referring generally to FIGS. 7A-14B, alternative example embodiments of components of the intervertebral implant system 100, for instance arcuate fixation member 12D, intervertebral implant spacers 316 and 336, and insert plate 350, are illustrated. Various embodiments of an intervertebral implant 400 can be constructed from the components of the intervertebral implant system 100, as described in more detail below. It should be noted preliminarily that in the interest of brevity, the figures and subsequent description pertaining to the arcuate fixation member 12D do not refer to certain features and/or uses of the arcuate fixation member 12C that may be integrated into the arcuate fixation member 12D, for example the use of the arcuate fixation member 12C in combination with above-described components of the intervertebral implant system 100, for instance the intervertebral implant spacer 108, the insert plate 116, the blocking plate 132, or the locking screw 138. However, embodiments in which those and other features of the arcuate fixation member 12C are integrated into the arcuate fixation member 12D are intended to be within the scope of the instant disclosure.

Referring now to FIGS. 7A-J, an alternative embodiment of the arcuate fixation member is illustrated. The arcuate fixation member 12D includes a fixation body, or body 300 defining a proximal end 300a, a distal end 300b opposite the proximal end, and an intermediate portion 300c extending between the proximal and distal ends 300a-b, respectively. The fixation body 300 has a cross sectional geometry that is substantially hexagonal, defining opposing laterally convex front and rear surfaces 300e-f extending between opposing sides, or edges 300d. The fixation body 300 defines a cross sectional geometry that is substantially constant throughout

11

the intermediate portion **300c** of the fixation body **300**, and is tapered between lateral surfaces **301** converging along the edges **300d** near the distal end **300b**, defining a tip **302** configured to cut into an underlying structure, such as bone. The intermediate portion **300c** of the fixation body **300** is curved along a central curved axis L1. It should be appreciated that the central curved axis L1 can define an insertion trajectory of the arcuate fixation member **12D** into underlying structure, such as a vertebral body. It should be appreciated that the insertion trajectory can be differently defined, for example in accordance with alternative geometries of the arcuate fixation member **12D**. In an embodiment, the intermediate portion **300c** is curved along substantially the entire length of the fixation body **300** between the proximal and distal ends **300a-b**, respectively. Alternatively, one or more distinct portions of the intermediate portion **300c** can be curved (not shown).

In the illustrated embodiment, the intermediate portion **300c** is curved along the central curved axis L1 in accordance with a uniform radius of curvature R1. Alternatively, the intermediate portion **300c** can define a non-uniform radius of curvature along the central curved axis L1. In a preferred embodiment, the curvature of the intermediate portion **300c** may be smooth and continuous. Alternatively, the curvature of the intermediate portion **300c** can be defined by a series of substantially straight sections (not shown), with each substantially straight section aligned along an individual longitudinal axis corresponding to the respective individual section, where the magnitude of an angle α with respect to a perpendicular reference axis A extended from the proximal end **300a** increases in magnitude with the distance of each subsequent straight section from the proximal end **300a**. It should be appreciated that the cross sectional geometry of the fixation body **300** is not limited to the illustrated substantially hexagonal shape, and that the fixation body **300** can alternatively be defined with any suitable cross sectional geometry. It should further be appreciated that the cross sectional dimension of the fixation body **300** may vary, for example increasing or decreasing, throughout one or more portions of the intermediate portion **300c**.

The arcuate fixation member **12D** may have a head **304** defined at the proximal end **300a** of the fixation body **300**. The head **304** may extend radially outward from the proximal end **300a** of the fixation body **300** in a direction perpendicular to the central curved axis L1. In an example embodiment, the head **304** may extend from the fixation body **300** in a direction generally towards the direction of curvature of the fixation body **300**, as depicted in FIGS. 7A-D. In alternative embodiments, the head **304** may extend from the fixation body **300** in a direction generally opposite from the direction of curvature of the fixation body **300**. The head **304** may define an upper surface **304a** configured for multi-angular engagement with a complementary surface of a delivery instrument, and a lower surface **304b** opposite the upper surface **304a** and configured to engage another component of the intervertebral implant system **100**, for example the insert plate **350**, when the arcuate fixation member **12D** is in an inserted position. The head **304** can have one or more tapered surfaces, for instance surface **304c**, defined thereon, the tapered surface **304c** configured to engage with a complementary surface in another component of the intervertebral implant system **100**, for example the insert plate **350**, thereby locking the arcuate fixation member **12D** in an inserted position.

The fixation body **300** can define one or more guidance members, the guidance members configured to guide the tip

12

302 along an insertion trajectory as the arcuate fixation member **12D** is inserted into an underlying structure, such as a vertebral body. In the illustrated embodiments, guidance members are disposed at distal end **300b** of the fixation body **300**, and in particular near the tip **302**, but can alternatively be defined at any location on the fixation body **300**. The fixation body **300** can define guidance members that are recessed within the fixation body **300**, such as the illustrated flutes **306**, or guidance members that comprise projections extending from the fixation body **300**, such as the illustrated outer wings **303** and/or the keel **308**, in any combination. For example, in the illustrated embodiment, a pair of recessed guidance flutes, or flutes **306** are defined by a keel **308** disposed between opposing wings **303**.

The illustrated flutes **306** are defined by and are disposed at the tip **302** of the fixation body **300**, the flutes **306** extending into the fixation body **300** from the tip **302** along directions substantially parallel to each other and to the insertion trajectory of the arcuate fixation member **12D**, and terminating in the intermediate section **300c** of the fixation body **300** proximal from the tip **302**. In alternative embodiments, the flutes **306** can extend along directions that are angularly offset or otherwise non-parallel with respect to each other and/or with respect to the insertion trajectory. The flutes **306** are not limited to the illustrated length, and can alternatively be defined to terminate within the tip **302** of the fixation body, or to extend along any length, up to the entirety, of the fixation body **300**. It should be appreciated that the flutes **306** can be symmetrically with respect to each other as illustrated, or asymmetrically. For example the flutes **306** can be defined with matching or different geometries, equal or different lengths, equal or different depths, etc.

The illustrated flutes **306** have a substantially "V" shaped geometry defined by outer wings, or wings **303** defined in the fixation body **300** and inner surfaces, or keel surfaces **305** defined in the fixation body **300**, the wings **303** and keel surfaces **305** converging in troughs **307**. The keel surfaces **305** define a keel **308**, as described in more detail below, the flutes **306** are disposed between respective wings **303** and the keel **308**. It should be appreciated that the wings **303** are not limited to the illustrated offset wings **303** disposed adjacent the keel **308** on respective sides of the keel **308**, and that a single, up to a plurality of wings **303** can be defined at any location in the fixation body **300**, for example substantially centrally between the edges **300d**, offset laterally toward either edge **300d**, or substantially along either edge **300d**. It should further be appreciated that the wings **303** and/or the keel surfaces **305** are not limited to being defined within the cross sectional geometry of the fixation body **300**, and can alternatively be defined to extend outwardly from the fixation body **300**, for example from the front or rear surfaces **300e-f** and/or the edges **300d**. It should further still be appreciated that the geometries of the flutes **306** are not limited to the illustrated "V" shape, and can alternatively be defined with any suitable geometry.

The keel surfaces **305** define a projection from the fixation body **300**, the projection configured as a guidance member in the form of a guidance keel, or keel **308**. In the illustrated embodiment, the keel **308** is defined substantially centrally between the edges **300d** of the fixation body **300**, and disposed between the wings **303**. In alternative embodiments, the keel **308** can be laterally offset toward either edge **300d**. It should be appreciated that the arcuate fixation member **12D** is not limited to a single keel **308** as illustrated, and that the fixation body **300** can define a plurality of keels **308** at any locations in the fixation body **300**. It should

13

further be appreciated that the arcuate fixation member 12D is not limited to the illustrated configuration of guidance members, and that the fixation body 300 can be differently constructed with any number of wings 303, flutes 306, keels 308, or any other guidance members, in any combination.

The fixation body 300 of the arcuate fixation member 12D can define one or more gripping structures configured to be retain the arcuate fixation member 12D in an inserted position within an underlying structure, such as a vertebral body. The gripping structures can include protrusions defined on the fixation body 300, such as teeth, spikes, or similar structures. For example, in the illustrated embodiment, a plurality of teeth 310 are defined in rows on opposing sides of the fixation body 300, in particular in the intermediate portion 300c of the fixation body 300 along the edges 300d. The illustrated plurality of teeth 310 are defined by a corresponding plurality of substantially "V" shaped notches 312 defined along the edges 300d of the fixation body 300. In the illustrated embodiment, the notches 312 are defined in parallel directions with respect to each other, such that the magnitude of an angle β between each notch 312 and the perpendicular reference axis A is maintained. In alternative embodiments, the notches 312 can be defined in directions that are not parallel with respect to each other, for example such that the magnitude of the angle β increases with the distance of each successive notch 312 from the proximal end 300a of the fixation body 300.

It should be appreciated that the gripping structures are not limited to being defined along the edges 300d of the fixation body 300, and that gripping structures supplemental to, or in lieu of, the illustrated teeth 310 can alternatively be defined in any other suitable location on the fixation body 300. It should further be appreciated that the gripping structures are not limited to the gripping structure geometry of the illustrated teeth 310, and that the fixation body 300 can alternatively define any other suitable gripping structure geometry. It should further still be appreciated that the number and/or geometry of the gripping structures can be defined so to add bone growth surface area to the arcuate fixation member 12D.

One or more removal members can be defined in the fixation body 300 of the arcuate fixation member 12D, the removal members allowing for distraction of the arcuate fixation member 12D from an underlying structure, such as a vertebral body. For example, in the embodiment illustrated in FIGS. 7A-H, a pair of grooves 314 are defined at the proximal end 300a of the fixation body 300, the grooves 314 extending into the fixation body 300 from the edges 300d. The illustrated grooves 314 are sized to receive complementary members of a removal tool. In an alternative embodiment illustrated in FIGS. 7I-J, a single groove 314 is defined at the proximal end 300a of the fixation body 300, the groove 314 extending into the rear surface 300f. It should be appreciated that the arcuate fixation member 12D is not limited to the illustrated removal members, and that the fixation body 300 can be alternatively be defined with one or more other suitable removal members.

Referring now to FIGS. 8A-D, an alternative embodiment of the intervertebral implant spacer, or spacer is illustrated. The intervertebral implant spacer, or spacer 316 defines a spacer body, or body 318 configured to be implanted into an intervertebral space, the spacer body 318 having an outer wall 318c that defines an enclosed perimeter of the spacer body 318. In the illustrated embodiment, the outer wall 318c comprises an anterior wall 318a extending between opposing ends 318b, a posterior wall 318d opposite the anterior wall 318a, and opposing side walls 318e, the side walls 318e

14

extending between the ends 318b of the anterior wall 318a and the posterior wall 318d. The spacer body 318 defines an upper surface 318f, and a lower surface 318g opposite the upper surface. The outer wall 318c defines an aperture 322 extending into the spacer body 318 through at least one of the upper or lower surfaces 318f-g.

A portion, up to an entirety of the anterior wall 318a can be curved inwardly toward the posterior wall 318d, defining an apex of curvature, or apex 320 in the anterior wall 318a approximately midway between the opposing ends 318b, as depicted in FIGS. 8A-B. Of course the apex 320 can be defined at any other location along the anterior wall 318a. In alternative embodiments, the anterior wall 318a can be straight between the ends 318b, can be curved outwardly away from the posterior wall 318d, or can define one or more distinct straight portions and/or curved portions between the ends 318b, thereby defining a corresponding number of apices 320 along the anterior wall 318a. It should be appreciated that the shape of the perimeter of the spacer body 318 is not limited to the illustrated geometry, and that the outer wall 318c can be differently constructed to define an alternatively shaped perimeter geometry of the spacer body 318.

The spacer body 318 can further include an inner wall 318h, the inner wall 318h defined so as to divide the aperture 322 defined by the outer wall 318c into a plurality of apertures 322. For example, in the illustrated embodiment, the inner wall 318h divides the aperture 322 defined by the outer wall 318c into a pair of apertures 322. The illustrated inner wall 318h extends between the apex 320 of the anterior wall 318a and the outer wall 318c, in particular between the apex 320 and substantially the midpoint of the posterior wall 318d. At least one additional aperture 322 can be defined between the anterior wall 318a and an insert plate, such as insert plate 350 (See FIGS. 10A-F) when the insert plate 350 is coupled to the spacer 316. One or more of the plurality of apertures 322 can be filled with bone growth inducing substances, for example to allow bony growth ingress and/or egress with respect to the spacer 316 and to assist in fusion between the spacer 316 and adjacent vertebral bodies.

In alternative embodiments, the spacer body 318 can be differently constructed, thereby alternatively defining the plurality of apertures 322. For example, it should be appreciated that the inner wall 318h can alternatively be defined to extend between any respective locations on the anterior wall 318a and the outer wall 318c. It should further be appreciated that the spacer body 318 is not limited to a single inner wall 318h as illustrated, and that alternatively a plurality of inner walls 318h having any combination of straight or curved geometries can be defined, the inner walls 318h of the plurality of inner walls 318h extending between a single or multiple locations on the anterior wall 318a and a single or multiple corresponding locations on the outer wall 318c, extending between respective locations on one or more inner walls 318h and the outer wall 318c, extending between a single or multiple locations on the outer wall 318c, extending from a single or multiple locations on the anterior wall 318a in a generally outward direction away from the posterior wall 318d, or any combination thereof. It should further still be appreciated that the respective thicknesses of the anterior wall 318a, the outer wall 318c, and/or the inner wall 318h can be uniform, or can have one or more portions of varying thickness.

One or more portions, up to an entirety of surfaces of the spacer body 318, for instance interior surfaces such as the inner surfaces 318c' of the outer wall 318c and/or the inner surfaces 318h' of the inner wall 318h, can be configured to

15

allow bony ingrowth into the respective surfaces by bone growth inducing substances disposed into the apertures 322, for instance to enhance fusion between the spacer 316 and adjacent vertebral bodies and/or to provide a form of secondary fixation between an intervertebral implant 400 constructed with the spacer 316 and adjacent vertebral bodies. For example, one or more portions of the inner surface 318c' of the outer wall 318c can be recessed, defining respective cavities 324 therein. The cavities 324 can be open to respective apertures 322, such that the cavities 324 can be filled with bone growth inducing substances and/or to allow the above-described bony ingrowth into the cavities 324. It should be appreciated that the spacer body 318 is not limited to the illustrated cavities 324, and that the surfaces of the spacer body 318 can be differently constructed with any other geometries in order to allow body ingrowth.

The apertures 322 defined in the spacer body 318 can be configured to be in communication with each other, for example to facilitate biological communication between bone growth inducing substances in respective apertures 322 and/or to allow bony growth ingress and/or egress between the apertures 322. For example, one or more openings, such as openings 326 can be defined through the outer wall 318c and/or the inner wall 318h, the openings 326 placing two or more of the plurality of apertures 322 in communication with each other. In the illustrated embodiment, a pair of openings 326 are defined through the outer wall 318c, and in particular the anterior wall 318a. It should be appreciated that the spacer body 318 can alternatively configured to define one, up to a plurality of openings 326 through the outer wall 318c and/or the inner wall 318h at any locations along the outer wall 318c and/or the inner wall 318h.

The spacer 316 is configured to be coupled to an insert plate, such as insert plate 350. Coupling members can be defined on the spacer body 318, the coupling members configured to releasably mate with complementary coupling members of an insert plate. For example, in the illustrated embodiment, coupling members in the form of retaining grooves 328 are defined in the ends 318b of the anterior wall 318a, the retaining grooves 328 extending into the spacer body 318 from open ends 328a defined in the lower surface 318g and terminating in closed ends 328b near the upper surface 318f. The retaining grooves 328 are configured to receive complementary retaining members, such as the retaining members 356 defined on the insert plate 350, therein. The closed ends 328b of the retaining grooves 328 can operate to retain the retaining members 356 of an insert plate within the retaining grooves 328 and/or act as stops to ensure proper alignment between an insert plate and the spacer 316 during assembly. In an alternative embodiment, the spacer 316 can be constructed such that the retaining grooves 328 extend along the entirety of the body 318, such that both ends 328a-b are open.

Interlocking members can be defined on the coupling members, the interlocking members configured to be received in releasably locking engagement with complementary interlocking members defined on the retaining members 356 of the insert plate 350. For example, in the illustrated embodiment, interlocking members in the form of locking ridges 330 are defined in the retaining grooves 328, the locking ridges 330 sized to be received in releasably locking engagement within complementary locking grooves 358 defined on the retaining members 356 of the insert plate 350. In addition to locking the insert plate 350 into position with respect to the spacer 316, the interlocking members can be configured to facilitate a desired alignment in the transverse, or cranial-caudal direction between the insert plate

16

and the spacer 316. For example, the illustrated locking ridges 330 are located within the retaining grooves 328 at a location approximately equal to the height wise midpoint of the anterior wall 318a, thereby ensuring that when the retaining members 356 are inserted into the retaining grooves 328 such that the locking ridges 330 are received in the locking grooves 358 (see FIG. 11B), the spacer 316 and the insert plate will achieve a desired transverse alignment with respect to each other.

The upper and lower surfaces 318f-g of the spacer body 318 can define a plurality of relief members, such as relief grooves 332, the relief grooves 332 configured to align with guide apertures 366 of the insert plate 350 (see FIGS. 10A-E) and to partially receive the fixation bodies 300 of respective arcuate fixation members 12D therein when an intervertebral implant 400 is assembled from the spacer 316 and an insert plate 350 and one or more arcuate fixation members 12D are inserted into the guide apertures 366 of the insert plate 350 and driven into position in an underlying structure, such as a vertebral body. In the illustrated embodiment, the relief grooves 332 are concave and are substantially smooth and devoid of any protrusions. It should be appreciated that the spacer 316 can be alternatively constructed without the relief grooves 332.

The upper and lower surfaces 318f-g of the spacer body 318 can be configured as bone-engaging surfaces, for example by defining gripping structures thereon, such as teeth, spikes, or the like. The gripping structures can be configured to engage adjacent underlying structures, such as the endplates of adjacent vertebral bodies, when the intervertebral implant 400 is inserted into an intervertebral space. In the illustrated embodiment, the upper and lower surfaces 318f-g have teeth 334 defined thereon. The teeth 334 may be pyramidal, saw toothed or other similar shapes. In alternative embodiments of the spacer 316, portions of, up to the entirety of the upper and/or lower surfaces 318f-g can be substantially smooth and devoid of any gripping structures.

The upper perimeter edge, or upper edge 318f and the lower perimeter edge, or lower edge 318g' of the spacer body 318, defined along the outer periphery of the spacer body 318 where the outer surface of the outer wall 318c intersects with the upper and lower surfaces 318f-g, respectively, can be rounded. Rounding the upper and lower edges 318f-g' can facilitate easier insertion and/or removal of the spacer 316, and thus the intervertebral implant 400, from an intervertebral space, for example by minimizing required distraction of the end plates of adjacent vertebral bodies. Distinct portions, up to an entirety of the upper and lower edges 318f-g' can be rounded using a varying radius of curvature. For example, in the illustrated embodiment respective portions of the upper and lower edges 318f-g' along the posterior wall 318d are rounded with a greater radius of curvature than the remainder of the upper and lower edges 318f-g', such that a "bullet tip" profile is defined on the posterior wall 318d of the spacer body 318, as depicted in FIG. 8D. In alternative embodiments, the upper and lower edges 318f-g' can be rounded using a substantially constant radius of curvature.

The upper and lower surfaces 318f-g can be defined as partially, up to fully convex surfaces. In the illustrated embodiment, the convexity of the upper and lower surfaces 318f-g in the anterior-posterior direction between the anterior wall 318a and the posterior wall 318d differs from the convexity of the upper and lower surfaces 318f-g in the lateral direction between the side walls 318e. The upper and lower surfaces 318f-g are fully convex in the anterior-posterior direction, and exhibit asymmetric convexity with

17

respect to each other, wherein the anterior-posterior convexity of the upper surface **318f** is defined using a shorter radius than the radius used to define the convexity of the lower surface **318g**. In other words, the upper surface **318f** exhibits a greater amount of curvature than the lower surface **318g**. The upper and lower surfaces **318f-g** are partially convex in the lateral direction, and exhibit symmetric convexity with respect to each other, wherein the lateral convexities of the upper and lower surfaces **318f-g** are equal, or mirror images of each other. In particular, the upper and lower surfaces **318f-g** define substantially no convexity in the lateral direction throughout the region C2, and are convex in the lateral direction in the regions C1 near the side walls **318e**.

It should be appreciated that the geometry of the upper and lower surfaces **318f-g** is not limited to the convexity of the illustrated embodiment, and that the upper and lower surfaces **318f-g** can be defined with full or partial convexity in the anterior-posterior and/or lateral directions, with full or partial concavity in the anterior-posterior and/or lateral directions, with a combination of partial convexity and concavity in the anterior-posterior and/or lateral directions, or with no curvature at all (i.e., substantially flat) in the anterior-posterior and/or lateral directions. It should further be appreciated that the regions C1 and C2 can be defined with wider or narrower widths in the lateral direction. It should further still be appreciated that the geometry of the upper and lower surfaces **318f-g** can be defined either symmetrically or asymmetrically with respect to each other.

Referring now to FIGS. 8C-D, the illustrated embodiment of the spacer **316** has a generally wedge shaped side view profile defined by a gradual increase in height followed by a gradual decrease in height between the anterior wall **318a** and the posterior wall **318d**, and a generally rectangular front view profile defined by a generally constant height throughout the C2 region, and gradually decreasing height throughout the C1 regions between the opposing ends of the C2 region and the side walls **318e**. In alternative embodiments the height between the anterior wall **318a** and the posterior wall **318d** of the spacer **316** may gradually decrease, may gradually increase, may have a gradual decrease followed by a gradual increase, or may be generally constant, while the height between the side walls **318e** may increase and/or decrease, or may be generally constant.

The geometry of the spacer **316**, for instance the geometry of the upper and lower surfaces **318f-g** and/or the difference in the height of the body **318** between the anterior and posterior walls **318a**, **318d** defines a lordotic angle θ of the spacer **316**. The lordotic angle θ defined by the spacer **316** can be increased and/or decreased by varying the geometry of the spacer **316**. For example, the lordotic angle θ defined by the illustrated spacer **316** can be increased by heightening the anterior wall **318a** of the spacer **316** while maintaining the height of the posterior wall **318d**. In preferred embodiments, the anterior-posterior convexity defined by the upper surface **318f** is increased with increasing magnitude of the lordotic angle θ , while the anterior-posterior convexity defined by the lower surface **318g** is maintained. It should be appreciated that when the geometry of the spacer **316** is alternatively constructed in order to increase or decrease the lordotic angle θ defined by the spacer **316**, the anterior-posterior convexity and/or the lateral convexity of the upper and/or lower surfaces **318f-g** can be increased or decreased in any combination such that the upper and lower surfaces **318f-g** are defined the same or differently.

Referring now to FIGS. 9A-D, another alternative embodiment of the intervertebral implant spacer, or spacer is illustrated. The intervertebral implant spacer, or spacer **336**

18

defines a generally hollow spacer body, or body **338** having an open anterior end **338a** defined between opposing ends **338b**, an outer wall **338c** extending around a perimeter of the spacer body **336** between the ends **338b**, and opposing upper and lower plates **338f-g**, the outer wall **338c** extending between the upper and lower plates **338f-g**. The upper and lower plates **338f-g** define respective upper and lower surfaces **338h-i**. In the illustrated embodiment, the outer wall **338c** is defined by a posterior wall **338d** opposite the anterior end **338a** and opposing side walls **338e**, the side walls **338e** extending between the ends **338b** and the posterior wall **338d**. It should be appreciated that the shape of the perimeter of the spacer body **338** is not limited to the illustrated geometry, and that the outer wall **338c** can be differently constructed to define an alternatively shaped perimeter geometry of the spacer body **338**.

The spacer body **338** can have a plurality of openings, such as apertures **340** and/or slots **342** defined therethrough, for example to allow bony growth ingress and/or egress with respect to the spacer body **338**, the bony growth ingress and/or egress assisting in fusion between the spacer **336** and adjacent vertebral bodies and/or providing a form of secondary fixation between an intervertebral implant **400** constructed with the spacer **336** and adjacent vertebral bodies. In the illustrated embodiment, a plurality of apertures **340** are defined extending through the upper and lower plates **338f-g**, and a plurality of slots **342** are defined extending through the outer wall **338c**. The apertures **340** that extend through each of the respective plates can have varying diameters with respect to each other and extend through the plates at locations that define a pattern that can be repeated between the upper and lower plates **338f-g** such that the each of the apertures **340** that extend through the upper plate **338f** are aligned with corresponding apertures that extend through the lower plate **338g** with respect to central axes defined between respective apertures in a substantially transverse direction to the spacer body **338**. The slots **342** are equally sized and elongate in the transverse direction between the upper and lower plates **338f-g**, and are spaced equally from each other along the outer wall **338c**.

The generally hollow interior of the spacer body **338** can be filled with bone growth inducing substances, for example to allow bony growth ingress and/or egress with respect to the spacer body **338** as described above. It should be appreciated that spacer body **338** is not limited to the illustrated apertures **340**, that the upper and lower plates **338f-g** can alternatively be defined with any number of apertures **340** of varying diameters and/or locations, and that the apertures **340** on the upper and lower plates **338f-g**, respectively, can be defined the same or differently. It should further be appreciated that the spacer body **338** is not limited to the illustrated slots **342**, that the outer wall **338c** can alternatively be defined with any number of slots **342** of varying shapes and/or sizes, and that the slots **342** can be spaced apart from each other equally or differently. It should further still be appreciated that the openings defined in the spacer body **338** are not limited to the illustrated apertures **340** and slots **342**, and that openings having any other geometry can be defined through the spacer body **338** at any respective locations, in addition to or in lieu of the apertures **340** and slots **342**. It should further still be appreciated that the respective thicknesses of the upper plate **338f**, the lower plate **338g** and/or the outer wall **338c** can be uniform or can have one or more portions of varying thickness.

The spacer **336** is configured to be coupled to an insert plate, such as insert plate **350**, such that the open anterior end **338a** is disposed between the posterior end **338d** and the

insert plate. Coupling members can be defined on the spacer body 338 of the spacer 336, the coupling members configured to releasably mate with complementary coupling members of an insert plate. For example, in the illustrated embodiment, coupling members in the form of retaining grooves 344 are defined in the ends 338*b* of the anterior end 338*a*, the retaining grooves 344 extending into the spacer body 338 from open ends 344*a* defined in the lower surface 338*i* and terminating in closed ends 344*b* near the upper surface 338*h*. The retaining grooves 344 are configured to receive complementary retaining members, such as the retaining members 356 defined on insert plate 350, therein. The closed ends 344*b* of the retaining grooves 344 can operate to retain the retaining members 356 of an insert plate within the retaining grooves 344 and/or act as stops to ensure proper alignment between an insert plate and the spacer 336 during assembly. In an alternative embodiment, the spacer 336 can be constructed such that the retaining grooves 344 extend along the entirety of the body 338, such that both ends 344*a-b* are open.

Interlocking members can be defined on the coupling members, the interlocking members configured to be received in releasably locking engagement with complementary interlocking members defined on the retaining members 356 of the insert plate 350. For example, in the illustrated embodiment, interlocking members in the form of locking ridges 346 are defined in the retaining grooves 344, the locking ridges 346 sized to be received in releasably locking engagement within complementary locking grooves 358 defined on the retaining members 356 of the insert plate 350. In addition to locking the insert plate 350 into position with respect to the spacer 336, the interlocking members can be configured to facilitate a desired alignment in the transverse, or cranial-caudal direction between the insert plate and the spacer 336. For example, the illustrated locking ridges 346 are located within the retaining grooves 344 at a location approximately equal to the height wise midpoint of the anterior end 338*a*, thereby ensuring that when the retaining members 356 are inserted into the retaining grooves 344 such that the locking ridges 346 are received in the locking grooves 358 (see FIG. 11B), the spacer 336 and the insert plate will achieve a desired transverse alignment with respect to each other.

The upper and lower plates 338*f-g* of the spacer body 338 can define a plurality of relief members, such as relief grooves 339, the relief grooves 339 configured to align with guide apertures 366 of the insert plate 350 (see FIGS. 10A-E) and to partially receive the fixation bodies 300 of respective arcuate fixation members 12D therein when an intervertebral implant 400 is assembled from the spacer 336 and an insert plate 350 and one or more arcuate fixation members 12D are inserted into the guide apertures 366 of the insert plate 350 and driven into position in an underlying structure, such as a vertebral body. In the illustrated embodiment, the relief grooves 339 define edges 339*a* in the upper and lower surfaces 338*h-i* that are substantially smooth and devoid of any protrusions. It should be appreciated that the spacer 336 can be alternatively constructed without the relief grooves 339.

The upper and lower surfaces 338*h-i* of the spacer body 338 can be configured as bone-engaging surfaces, for example by defining gripping structures thereon, such as teeth, spikes, or the like. The gripping structures can be configured to engage adjacent underlying structures, such as the endplates of adjacent vertebral bodies, when the intervertebral implant 400 is inserted into an intervertebral space. In the illustrated embodiment, the upper and lower surfaces

338*h-i* have teeth 348 defined thereon. The teeth 348 may be pyramidal, saw toothed or other similar shapes. In alternative embodiments of the spacer 336, portions of, up to the entirety of the upper and/or lower surfaces 338*h-i* can be substantially smooth and devoid of any gripping structures.

The upper perimeter edge, or upper edge 338*h'* and the lower perimeter edge, or lower edge 338*i'* of the spacer body 338, defined along the outer periphery of the spacer body 338 where the outer surface of the outer wall 338*c* intersects with the upper and lower surfaces 338*h-i*, respectively, can be rounded. Rounding the upper and lower edges 338*h'-i'* can facilitate easier insertion and/or removal of the spacer 336, and thus the intervertebral implant 400, from an intervertebral space, for example by minimizing required distraction of the end plates of adjacent vertebral bodies. Distinct portions, up to an entirety of the upper and lower edges 338*h'-i'* can be rounded using a varying radius of curvature. For example, in the illustrated embodiment respective portions of the upper and lower edges 338*h'-i'* along the posterior wall 338*d* are rounded with a greater radius of curvature than the remainder of the upper and lower edges 338*h'-i'*, such that a "bullet tip" profile is defined on the posterior wall 338*d* of the spacer body 338, as depicted in FIG. 9D. In alternative embodiments, the upper and lower edges 338*h'-i'* can be rounded using a substantially constant radius of curvature.

The upper and lower surfaces 338*h-i* can be defined as partially, up to fully convex surfaces. In the illustrated embodiment, the convexity of the upper and lower surfaces 338*h-i* in the anterior-posterior direction between the anterior end 338*a* and the posterior wall 338*d* differs from the convexity of the upper and lower surfaces 338*h-i* in the lateral direction between the side walls 338*e*. The upper and lower surfaces 338*h-i* are fully convex in the anterior-posterior direction, and exhibit asymmetric convexity with respect to each other, wherein the anterior-posterior convexity of the upper surface 338*h* is defined using a shorter radius than the radius used to define the convexity of the lower surface 338*i*. In other words, the upper surface 338*h* exhibits a greater amount of curvature than the lower surface 338*i*. The upper and lower surfaces 338*h-i* are partially convex in the lateral direction, and exhibit symmetric convexity with respect to each other, wherein the lateral convexity of the upper and lower surfaces 338*h-i* are equal, or mirror images of each other. In particular, the upper and lower surfaces 338*h-i* define substantially no convexity in the lateral direction throughout the region C4, and are convex in the lateral direction in the regions C3 near the side walls 338*e*.

It should be appreciated that the geometry of the upper and lower surfaces 338*h-i* is not limited to the convexity of the illustrated embodiment, and that the upper and lower surfaces 338*h-i* can be defined with full or partial convexity in the anterior-posterior and/or lateral directions, with full or partial concavity in the anterior-posterior and/or lateral directions, with a combination of partial convexity and concavity in the anterior-posterior and/or lateral directions, or with no curvature at all (i.e., substantially flat) in the anterior-posterior and/or lateral directions. It should further be appreciated that the regions C3 and C4 can be defined with wider or narrower widths in the lateral direction. It should further still be appreciated that the geometry of the upper and lower surfaces 338*h-i* can be defined either symmetrically or asymmetrically with respect to each other.

Referring now to FIGS. 9C-D, the illustrated embodiment of the spacer 336 has a generally wedge shaped side view profile defined by a gradual increase in height followed by a gradual decrease in height between the anterior end 338*a*

21

and the posterior wall **338d**, and a generally rectangular front view profile defined by a generally constant height throughout the C4 region, and gradually decreasing height throughout the C3 regions between the opposing ends of the C4 region and the side walls **338e**. In alternative embodiments the height between the anterior end **338a** and the posterior wall **338d** of the spacer **336** may gradually decrease, may gradually increase, may have a gradual decrease followed by a gradual increase, or may be generally constant, while the height between the side walls **338e** may increase and/or decrease, or may be generally constant.

The geometry of the spacer **336**, for instance the geometry of the upper and lower surfaces **338h-i** and/or the difference in the height of the body **338** between the anterior end **338a** and the posterior wall **338d** defines a lordotic angle θ of the spacer **336**. The lordotic angle θ defined by the spacer **336** can be increased and/or decreased by varying the geometry of the spacer **336**. For example, the lordotic angle θ defined by the illustrated spacer **336** can be increased by heightening the anterior end **338a** of the spacer **336** while maintaining the height of the posterior wall **338d**. In preferred embodiments, the anterior-posterior convexity defined by the upper surface **338h** is increased with increasing magnitude of the lordotic angle θ , while the anterior-posterior convexity defined by the lower surface **338i** is maintained. It should be appreciated that when the geometry of the spacer **336** is alternatively constructed in order to increase or decrease the lordotic angle θ defined by the spacer **336**, the anterior-posterior convexity and/or the lateral convexity of the upper and/or lower surfaces **338h-i** can be increased or decreased in any combination such that the upper and lower surfaces **338h-i** are defined the same or differently.

Referring now to FIGS. 10A-F, alternative embodiments of the insert plate are illustrated. The insert plate, or insert **350** defines a plate having plate body, or body **352** extending between opposing plate ends **352a**, the plate body **352** defining an anterior side **352b**, a posterior side **352c** opposite the anterior side, an upper surface **352d**, and a lower surface **352e** opposite the upper surface. In the illustrated embodiments, the anterior side **352b** defines a curved outer periphery of the plate body **352**. The plate body **352** can define one or more insert members, such as insert slots **354**, the insert members configured to receive the complementary members defined on a delivery, or insertion instrument. It should be appreciated that the insert members are not limited to the illustrated insert slots **354**, and that the insert members can be alternatively defined in accordance with the complementary insert members of a respective delivery instrument.

The insert plate **350** is configured to be coupled to a spacer, for instance the above-described spacers **316** or **336**. Coupling members can be defined on the plate body **352**, the coupling members configured to releasably mate with complementary coupling members of a spacer. For example, in the illustrated embodiments, coupling members in the form of retaining members **356** are defined on the insert plate **350**, the retaining members being generally “L” shaped, so as to be slidably received in the retaining grooves **328** or **344** of the spacers **316** or **336**, respectively. In the embodiments illustrated in FIGS. 10A-D and 10F, a “shallow” insert plate **350** is depicted, in which the retaining members **356** are defined on the plate ends **352a**, the retaining members **356** extending outwardly from the posterior side **352c** of the plate body **352**. When the shallow insert plate **350** is coupled to the spacer **316** (see FIG. 11A), an aperture **322** is defined between the anterior wall **318a** of the spacer body **318** of the spacer **316** and the posterior side **352c** of the plate body **352** of the shallow insert plate. In the

22

embodiment illustrated in FIG. 10E, a “deep” insert plate **350** is depicted, in which the retaining members **356** are defined at the ends of side walls **352f** that extend from the plate ends **352a**, the retaining members **356** extending outwardly from the ends of the side walls **352f**. When the deep insert plate **350** is coupled to the spacer **316**, an aperture **322** is defined between the anterior wall **318a** of the spacer body **318** of the spacer **316** and the posterior side **352c** and side walls **352f** of the plate body **352** of the shallow insert plate. The volume of the aperture **322** defined by the spacer **316** coupled to the deep insert plate **350** is greater than the volume of the aperture **322** defined by the spacer **316** coupled to the deep insert plate **350**.

Interlocking members can be defined on the coupling members, the interlocking members configured to receive complementary interlocking members, such as the retaining grooves **328** or **344** defined in the spacers **316** or **336**, respectively, in releasably locking engagement. For example, in the illustrated embodiments, interlocking members in the form of locking grooves **358** are defined in the ends of the retaining members **356**. The locking grooves define a height in the transverse direction, and are of sufficient height to receive the locking ridges **330** or **346** of the spacers **316** or **336**, respectively, therein. In addition to locking the insert plate **350** into position with respect to a spacer **316** or **336**, the interlocking members can be configured to facilitate a desired alignment in the transverse direction between the insert plate **350** and the respective spacer, as described above. In the illustrated embodiments the locking grooves **358** can define a height that is longer than the corresponding height of the locking ridges **330** or **346**, in order to allow for a limited amount of translation by the insert plate **350** and the respective spacer with respect to each other.

It should be appreciated that the insert plate **350** and spacers **316** and **336** are not limited to the illustrated configurations of the coupling members and/or interlocking members. For example, the retaining grooves **328** or **344** could be defined in the insert plate **350**, and the retaining members **356** could be defined on the spacers **316** or **336**. Similarly, the locking ridges **330** or **346** could be defined on the retaining members **356**, and the locking grooves **358** could be defined in the retaining grooves **328** or **344**. It should further be appreciated that the coupling members are not limited to the illustrated structures of the retaining grooves **328** and **344** or the retaining members **356**. For example, the respective orientations of the retaining grooves **328** or **344** and the retaining members **356** could be reversed with respect to the lateral direction. It should further still be appreciated that the insert plate **350** and spacers **316** and **336** are not limited to the illustrated coupling members and/or interlocking members, and that any alternative structures can be employed to couple and/or lock the spacers **316** or **336** and the insert plate **350** with respect to each other.

The upper and lower surfaces **352d-e** of the plate body **352** can be configured as bone-engaging surfaces, for example by defining gripping structures thereon, such as teeth, spikes, or the like. The gripping structures can be configured to engage adjacent underlying structures, such as the endplates of adjacent vertebral bodies, when the intervertebral implant **400** is inserted into an intervertebral space. In the embodiments illustrated in FIGS. 10A-D and 10F, portions of the upper and lower surfaces **352d-e** have teeth **360** defined thereon. The teeth **360** may be pyramidal, saw toothed or other similar shapes. In the embodiment illustrated in FIG. 10E, the entireties of the upper and lower surfaces **352d-e** have teeth **360** defined thereon. The upper

23

and lower edges **352d'-e'** of the upper and lower surfaces **352d-e**, respectively, can be rounded. Rounding the upper and lower edges **352d'-e'** can facilitate easier insertion and/or removal of the insert plate **350**, and thus the intervertebral implant **400**, from an intervertebral space, for example by minimizing required distraction of the end plates of adjacent vertebral bodies. Distinct portions, up to an entirety of the upper and lower edges **352d'-e'** can be rounded using substantially constant or varying radii of curvature.

The geometry of the upper and lower surfaces **352d-e** of the plate body **352** may be defined to generally conform the insert plate **350** to the geometry of the spacers **316** or **336**. For example, in the illustrated embodiments, the upper and lower surfaces **352d-e** are defined as partially convex surfaces. In particular, the upper and lower surfaces **352d-e** exhibit lateral convexity in the regions C5 near the plate ends **352a**, the convexity on the upper and lower surfaces **352d-e** being symmetric with respect to each other. The height of the insert plate **350** gradually decreases between the anterior and posterior sides **352b-c**, respectively (see FIGS. 12A-B). It should be appreciated that the insert plate **350** is not limited to the illustrated geometry of the upper and lower surfaces **352d-e**, and that the upper and lower surfaces **352d-e** can be defined with full or partial convexity in the anterior-posterior and/or lateral directions, with full or partial concavity in the anterior-posterior and/or lateral directions, with a combination of partial convexity and concavity in the anterior-posterior and/or lateral directions, or with no curvature at all (i.e., substantially flat) in the anterior-posterior and/or lateral directions. It should further be appreciated that the regions C5 can be defined with wider or narrower widths in the lateral direction. It should further still be appreciated that the geometry of the upper and lower surfaces **352d-e** can be defined either symmetrically or asymmetrically with respect to each other. It should further still be appreciated that the height of the insert plate **350** between the anterior and posterior sides **352b-c**, respectively, may gradually increase, may have a gradual decrease followed by a gradual increase, may have a gradual increase followed by a gradual decrease, or may be generally constant, and that the height between the plate ends **352a** may increase and/or decrease, or may be generally constant.

The anterior side **352b** of the plate body **352** can define a concave recess **362**, the recess configured to receive the complementary convex surface of a blocking plate, such as the blocking plate **132** described above. The insert plate **350** can also have a central bore **364** defined therethrough, the central bore **364** defining a threaded inner bore surface **364a**, the threads of the inner bore surface **364a** configured to engage complementary threads of a locking screw, such as the locking screw **138** described above.

The plate body **352** can also have one or more guide apertures **366** defined therethrough, the guide apertures **366** configured to slidably receive bone fixation members therein, such as the arcuate fixation members **12D**, and to define insertion trajectories into underlying structures for the fixation members received therein. In the illustrated embodiments, the guide apertures **366** are defined as substantially straight guide apertures extending through the plate body **352** from within the concave recess **362** in the anterior side **352b** through the posterior side **352c**. The guide apertures **366** can have substantially uniform cross sectional geometries that are defined to substantially conform to the cross sectional geometry of the intermediate portion **300c** of the body **300** of the arcuate fixation member **12D**.

The guide apertures **366** and/or the arcuate fixation members **12D** can be configured to releasably lock respective

24

arcuate fixation members **12D** in inserted positions within the guide apertures **366**. For example, in the illustrated embodiments, recessed ledges **368** are defined in the surface of the concave recess **362** around a portion of the perimeter of each of the guide apertures **366**, the recessed ledges **368** configured to receive the lower surfaces **304b** of the heads **304** of respective arcuate fixation members **12D** when the arcuate fixation members **12D** are inserted into respective guide apertures **366**. One or more surfaces within the recessed ledges **368** can be configured to engage with complementary tapered surfaces defined on the heads **304** of respective arcuate fixation members **12D**, for instance surfaces **304c**, thereby locking the arcuate fixation members **12D** in respective inserted positions. In an alternative embodiment, the cross sectional geometries of the guide apertures **366** can be tapered between the anterior and posterior sides **352b-c** of the plate body **352**, such that the arcuate fixation members **12D** are press fit within the guide apertures **366** as they are inserted. Of course the arcuate fixation members **12D** and/or the guide apertures **366** can be configured such that no locking affect is imparted therebetween. It should be appreciated that the above-described blocking plate **132** and locking screw **138** can be employed to secure the arcuate fixation members **12D** within inserted positions in the guide apertures, whether or not the arcuate fixation members **12D** and/or the guide apertures **366** are configured to releasably lock with respect to each other.

The guide apertures **366** can be disposed about the central bore **364** at any desired locations and can define any insertion trajectories as appropriate. In the illustrated embodiments, the guide apertures **366** are defined in opposing quadrants around the central bore **364**, with two guide apertures **366** located near the upper surface **352d** and defining two generally outward and cranial insertion trajectories, and two guide apertures **366** located near the lower surface **352e** and defining two generally outward and caudal insertion trajectories. It should be appreciated that the insert plate **350** is not limited to the illustrated configuration of guide aperture **366** locations and insertion trajectories, and that the insert plate **350** can be differently configured with any number of guide apertures **366** defined at any locations on the plate body **352** and having any insertion trajectories. It should further be appreciated that the guide apertures **366** can be straight, curved along one or more locations between the anterior and posterior sides **352b-c**, respectively, or any combination thereof.

Referring now to FIGS. 11A-12C, an example embodiment of an intervertebral implant **400** constructed from components of the intervertebral implant system **100** is illustrated. In particular, the intervertebral implant **400** includes an insert plate **350** coupled to a spacer **316**. The intervertebral implant **400** can further include one or more arcuate fixation members **12D**, a blocking plate **132**, and/or a locking screw **138** (see FIGS. 14A-B), for example in accordance with the insert plate **350** provided. It should be appreciated that the intervertebral implant **400** can be alternatively constructed with the spacer **336**, that the insert plate **350** can be provided as a shallow insert plate **350** or a deep insert plate **350** as described above, and that the insert plate **350** can be constructed with or without the guide apertures **366**. In the illustrated embodiment, the spacer **316**, and in particular the outer wall **318c**, is constructed so that the width W of the spacer **316** in the lateral direction substantially conforms to the width of the insert plate **350** in the lateral direction. The insert plate **350** coupled to the spacer **316** in the illustrated embodiment is a shallow insert plate **350**, as described above. When coupled to each other in an

25

assembled configuration, the spacer 316 and the insert plate 350 define a “footprint” of the intervertebral implant 400, the footprint referring to the shape of the outer periphery of the intervertebral implant 400 as defined by the outer wall 318c of the spacer 316 and the anterior side 352b of the insert plate 350.

It should be appreciated that the intervertebral implant 400 is not limited to the illustrated footprint, and that the spacer 316 and/or the insert plate 350 can be differently constructed to define alternative footprints of the intervertebral implant 400. For example, the deep insert plate 350, described above, can be coupled to the spacer 316 in lieu of the shallow insert plate 350, defining an intervertebral implant 400 having a larger footprint than the footprint defined by the shallow insert plate 350 coupled to the spacer 316 (see FIG. 12A). Additionally, when the deep insert plate 350 is coupled to the spacer 316, the aperture 322 defined by the anterior wall 318a of the spacer 316 and the posterior side 352c of the insert plate 350 is larger than the equivalent aperture 322 defined when the shallow insert plate 350 is coupled to the spacer 316. The spacer 316 can also be differently constructed, for example by defining the outer wall 318c with alternative widths W of the spacer 316 in the lateral direction and/or depths D of the spacer 316 in the anterior-posterior direction. For instance, the spacer 316 depicted in FIGS. 12B-C has a greater width and depth than the spacer 316 depicted in FIGS. 11A and 12A, thereby defining intervertebral implants 400 with larger footprints when coupled to the shallow or deep insert plates 350, as depicted in FIGS. 12B-C, respectively. It should be appreciated that the spacer 316 can similarly be differently constructed with varying widths and/or depths, thereby defining intervertebral implants 400 with differently sized footprints when coupled to the shallow or deep insert plates 350.

Referring now to FIGS. 13A-B, in addition to providing for the construction of intervertebral implants 400 defining varying footprints, the components of the intervertebral implant system 100 also provide for the construction of intervertebral implants 400 defining varying lordotic angles. The lordotic angle θ of an intervertebral implant 400 can be defined by the geometry of its component parts, such as the surface geometry of the components and/or the height of the components. In the embodiment illustrated in FIG. 13A, a spacer 316 is coupled to an insert plate 350 having a height that is shorter than the height of the spacer 316 at the ends 318b of the anterior wall 318a. The lordotic angle θ of the intervertebral implant 400 is defined by the spacer 316. In an alternative embodiment illustrated in FIG. 13B, the spacer 316 is identical to the spacer 316 used in constructing the intervertebral implant 400 depicted in FIG. 13A, but is coupled to an insert plate 350 having a height that is taller than the height of the spacer 316 at the ends 318b of the anterior wall 318a. The increased height of the insert plate 350 produces a corresponding increase in the magnitude of the lordotic angle θ of the intervertebral implant 400. It should be appreciated that the lordotic angle defined by intervertebral implants 400 constructed using the spacer 316 can similarly be varied based upon the height of the insert plate 350 coupled thereto. It should further be appreciated that the spacers 316 and/or 336 can be differently constructed with varying heights, thereby defining intervertebral implants 400 with different lordotic angles when coupled to identical insert plates 350.

Referring now to FIGS. 14A-B, an example intervertebral implant 400 is illustrated in an exploded view containing selected components of the intervertebral implant system 100, and in an assembled configuration after being inserted

26

into an intervertebral space, respectively. The characteristics of the assembled intervertebral implant 400, for instance the footprint and/or lordotic angle defined thereby, can be tailored when selecting the individual components, for example in accordance with region of the spine where the intervertebral implant 400 will be inserted, particular patient anatomy, and the like. Thus, the intervertebral implant system 100 can be described as a modular intervertebral implant system 100 that allows a surgeon to construct a patient specific intervertebral implant 400. In the illustrated example, the spacer 316 and insert plate 350 can be selected based upon the desired footprint and/or lordotic angle that will be defined by the intervertebral implant. The quantity and length of arcuate fixation members 12C and/or 12D can also be selected.

Once the components of the intervertebral implant system 100 have been selected, the spacer can be coupled to the insert plate by inserting the retaining members of the insert plate into the retaining grooves on the spacer and advancing the retaining members until the locking ridges are received in the locking grooves. The intervertebral implant 400 can then be filled with bone growth inducing substances as described above and inserted into an intervertebral space between adjacent vertebral bodies using an insertion, or delivery instrument (not shown). The arcuate fixation members can then be inserted into the guide apertures and driven into place within the adjacent vertebral bodies. Once the arcuate fixation members are inserted, a blocking plate can be disposed into the concave recess in the insert plate and a locking screw can be driven through the blocking plate and into the insert plate, thereby securing the intervertebral implant in an assembled and inserted configuration.

It should be appreciated that a variety of kits can be provided that contain one or more components of the intervertebral implant system 100. The components of the kits may be configured the same or differently. For example, within a single kit, arcuate fixation members 12C and/or 12D may be provided that have different lengths, different radii of curvature, differing head configurations, differing cross sectional geometries, and so on, depending for example on the type of procedure being performed by a surgeon, or on the particular anatomies of individual patients. The kits may also be configured differently with respect to which components of the intervertebral implant system 100 are included in the kits. For example, a kit for the intervertebral implant system 100 may include arcuate fixation members 12C and/or 12D of different lengths, radii of curvature, and/or features, and may include one or more of spacers 108, 316 and/or 336 having different heights, perimeter geometries, or surface geometries, or defining different lordotic angles, insert plates 116 or 350 having different heights, perimeter geometries, surface geometries, and guide apertures, blocking plates 132, or locking screws 138.

Although arcuate fixation members and the other components of the intervertebral implant system 100 have been described herein with reference to preferred embodiments or preferred methods, it should be understood that the words which have been used herein are words of description and illustration, rather than words of limitation. For example, it should be noted that although the intervertebral implant system 100 has been described herein with reference to particular structure, methods, and/or embodiments, the scope of the instant disclosure is not intended to be limited to those particulars, but rather is meant to extend to all structures, methods, and/or uses of the intervertebral implant system 100. Those skilled in the relevant art, having the benefit of the teachings of this specification, may effect

27

numerous modifications to the intervertebral implant system **100** as described herein, and changes may be made without departing from the scope and spirit of the instant disclosure, for instance as recited in the appended claims.

What is claimed:

1. A method for fixing an intervertebral implant in an intervertebral space defined between an upper vertebral body and a lower vertebral body, the method comprising the steps of:

inserting the intervertebral implant into the intervertebral space, the intervertebral implant including a spacer body and a fixation plate coupled to the spacer body, the fixation plate defining a plurality of guide apertures extending therethrough; and

inserting a plurality of curved bone fixation members into respective ones of the plurality of guide apertures such that at least one curved bone fixation member of the plurality of curved bone fixation members is rotationally fixed in a respective at least one of the plurality of guide apertures as the at least one curved bone fixation member is inserted into engagement with at least one of the upper and lower vertebral bodies such that, the plurality of curved bone fixation members fix the intervertebral implant to the at least one of the upper and lower vertebral bodies;

wherein the inserting step includes guiding the at least one curved bone fixation member along an insertion trajectory through the at least one of the upper and lower vertebral bodies via a guidance member disposed at least partially along a distal end of the at least one curved bone fixation member, the guidance member including a keel, a first wing disposed adjacent the keel, and a second wing adjacent the keel opposite the first wing, where the keel and the first and second wings guide the at least one curved bone fixation member along the insertion trajectory.

2. The method of claim 1, wherein each of the plurality of curved bone fixation members is elongate along a curved fixation member axis, and the step of inserting the plurality of curved bone fixation members into the respective ones of the plurality of guide apertures further comprises inserting the plurality of curved bone fixation members along respective curved trajectories into the at least one of the upper and lower vertebral bodies.

3. The method of claim 1, further comprising locking each of the plurality of curved bone fixation members to the fixation plate.

4. The method of claim 1, further comprising, prior to inserting the intervertebral implant into the intervertebral space, packing the spacer body with a bone growth material.

5. The method of claim 1, further comprising coupling the fixation plate to the spacer body.

6. The method of claim 1, wherein the step of inserting the plurality of curved bone fixation members into the respective ones of the plurality of guide apertures includes translating each of the plurality of curved bone fixation members along a respective guide aperture of the plurality of guide apertures.

7. The method of claim 6, wherein the spacer body defines an upper vertebra facing surface and an opposed lower vertebra facing surface, the plurality of guide apertures includes at least one upper guide aperture that extends toward the upper vertebra facing surface of the spacer body, and the step of inserting the plurality of curved bone fixation members into the respective ones of the plurality of guide apertures includes:

28

inserting at least one first curved bone fixation member through the at least one upper guide aperture and into engagement with the upper vertebral body.

8. The method of claim 7, wherein the plurality of guide apertures includes at least one lower guide aperture that extends toward the lower vertebra facing surface of the spacer body, and the step of inserting the plurality of curved bone fixation members into the respective ones of the plurality of guide apertures includes:

inserting at least one second curved bone fixation member of the plurality of curved bone fixation members into the at least one lower guide aperture and into engagement with the lower vertebral body.

9. The method of claim 8, further comprising securing a blocking plate to the fixation plate such that the blocking plate prevents the plurality of the curved bone fixation members from backing out of the respective ones of the plurality of curved guide apertures.

10. The method of claim 1, further comprising: selecting one of a plurality of spacer bodies, at least a pair of the plurality of spacer bodies defining a different at least one of a size and shape; and coupling one of a plurality of fixation plates to the selected one of the plurality of spacer bodies so as to define the intervertebral implant.

11. The method of claim 1, wherein the spacer body includes at least one aperture extending therethrough.

12. The method of claim 1, wherein the spacer body includes an upper plate and a lower plate, the upper plate defines an upper surface, and the lower plate defines a lower surface, the spacer body being a hollow spacer body defining a hollow region that extends between the upper and lower plates.

13. The method of claim 12, further comprising packing the hollow spacer body with a bone growth material.

14. The method of claim 1, wherein the spacer body defines 1) an upper surface, 2) an opposed lower surface, and 3) an outer wall that extends from the upper surface to the lower surface, the outer wall at least partially defining a pair of apertures that each extends through the upper and lower surfaces, the spacer body further including an inner wall that separates one of the pair of apertures from the other of the pair of apertures, wherein the method includes,

positioning the fixation plate on the spacer body so that the fixation plate and the outer wall define an additional aperture therebetween, the additional aperture being aligned with the inner wall.

15. The method of claim 14, further comprising packing the pair of apertures with a bone growth material.

16. The method of claim 1, wherein the at least one curved bone fixation member defines a proximal end, a distal end spaced from the proximal end along a curved fixation member axis, and a curved fixation body extending along the curved fixation member axis, the curved fixation body defining a cross-sectional shape that conforms to the respective at least one of the plurality of guide apertures such that the curved fixation body is rotatably fixed in the respective at least one of the plurality of guide apertures when inserted into the respective at least one of the plurality of guide apertures.

17. The method of claim 16, wherein the distal end defines a tapered tip that extends distally from the curved fixation body, the tapered tip configured to cut into the respective upper and lower vertebral bodies.

18. The method of claim 17, wherein the curved fixation body defines a first cross-sectional dimension that is perpendicular to the curved fixation member axis, a second

29

cross-sectional dimension that is perpendicular the first cross-sectional dimension, and a third cross-sectional dimension that is perpendicular to the first and second cross-sectional dimensions, wherein the first, second and third cross-sectional dimensions pass through the curved fixation member axis, and the tapered tip tapers from each of the first, second and third cross-sectional dimensions toward the curved fixation member axis.

19. The method of claim 1, wherein the plurality of guide apertures are curved.

10

* * * * *

30